

Chapter 2

Skeletal Muscle

Abstract This chapter is an update of the current view of the general structure and function of the human skeletal muscle system with its functional muscle groups (e.g., antigravity muscles) with special emphasis on the almost forgotten muscular reinforcement structures (fascia and entheses) and on the myocellular force-producing little power chambers inside skeletal muscle fibers known as sarcomeres. Skeletal muscle is well adapted to gravitational loading (1G) on Earth but is highly challenged to microgravity unloading in Space (μ G, zero-G). In particular, we found that nitric oxide (NO) signaling and nitrosative stress management (via protein S-nitrosylation) in human skeletal muscle provide reliable signatures to assess efficacy of physical countermeasures. We use high-resolution confocal laser microscopy for the precise immunohistochemical biomarker detection at the cellular and subcellular level combined with quantitative biochemical methods and current protein mapping by 2-DIGE proteomics to comprehensively document disuse changes in normal healthy muscle and to assess efficacy of different exercise countermeasures against disuse atrophy. Over more than 10 years, our laboratory cooperates with national and international multidisciplinary Space Life Sciences research groups in ground-based experiments (mice) and in several bed rest studies, for example, using resistive vibration exercise (RVE) as a very efficient countermeasure against chronic disuse. Published and preliminary results from two long- and medium-term spaceflight experiments with mice, one on the International Space Station (91 days MDS mission) and another one on a Russian biosatellite on orbit (30 days BION M1 mission), provided new insights to cell signaling changes in mammalian skeletal muscle in real microgravity.

Keywords Skeletal muscle • Nitric oxide signaling • Nitrosative stress • Ground-based experiments • Physical countermeasure • Spaceflight

2.1 Skeletal Muscle Structure and Function

2.1.1 *Functional Anatomy of Normal Human Skeletal Muscle*

The human skeletal muscle system comprises about 220 specific muscles with various sizes, shapes, locations, and functions in the body. Some are relatively small (<3 cm in length) such as some hand and foot muscles (interossei, lumbricales) used for complex finger/toe movement control (grasping, playing on instruments) or some deep medial column back muscles (rotators) for local segmental spine rotations. Some are even smaller (<3 mm) and used for fine-tuning of discrete movements (Alkner and Tesch 2004) (e.g., the little stapedius controls movements of the last of three middle ear bones) in acoustic sensation and hearing. Others are longer (>40 cm, sartorius, erector spinae), while others are broader and rather powerful and fleshy (quadriceps femoris, latissimus dorsi, adductors) for use in body stabilization (posture, gait) and mobilization (movements, performance). Another functional group is located at deep muscle layers adjacent to bones running closely over one or more joints (single vs. multi-joint muscles) to facilitate local joint movement and stabilization (see Sect. 2.1.4). In general, almost 60 % of the functional skeletal musculature in the healthy human body is used for body stabilization and postural control during stance and body motions in normal everyday life on Earth and is thus termed “antigravity” muscles (Fig. 2.1).

Most of the skeletal muscles are usually grouped in the body by anatomic and functional compartments classified according to their body location and function in the trunk or extremities as ventral/dorsal, medial/lateral, and extensor/flexor compartments. For example, the soleus and gastrocnemius belong to the superficial dorsal calf plantar flexors (triceps surae) which insert via the Achilles tendon to the calcaneus bone (Fig. 2.1). The adductor muscles (short, long, and greater adductor, gracilis) belong to the medial thigh compartment (thigh adductors) for hip stabilization and leg adduction. Muscle compartments are located underneath the main body fascia (similar to a whole body stocking or cat suit) separated from the skin above (Schleip et al. 2012). The muscle compartments underneath the main body fascia particularly of the arms and legs resemble long spaces separated by fibrous connective tissue sheets known as fascia sheets or box fascia which usually contain about two or three individual muscles (e.g., the long and short fibularis of the lateral calf compartment) or two-/three-headed single muscles (e.g., biceps/triceps of ventral arm flexors/dorsal arm extensors). Each compartment is comparable to a box with functionally grouped (extensor/flexor/adductor) muscles that receive a common neurovascular supply (nerve and blood vessels) from deep main arteries or peripheral nerves and thus participate in the functional anatomy of human skeletal muscle (Blottner 2013). In most body regions, the fascia layers are part of the soft muscle tissue (Fig. 2.2) and may not be easily palpable, while others are more stiff (i.e., great thoracolumbar fascia) and well palpable on the back superficial lumbar region or at the lateral hip region (iliotibial tract) of the lower limb.

Anti-Gravity-Muscles of the Human Body (Postural Muscles)

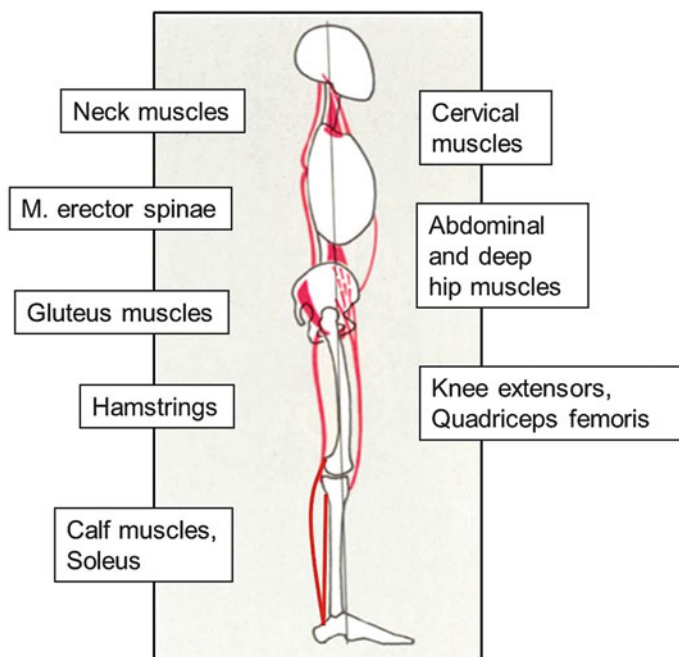


Fig. 2.1 Cartoon showing the key “antigravity” skeletal muscle groups of the human body for postural control of body stabilization, during stance, gait, and other motions/movements on Earth (1G)

The Myofascial Tension and Support System Muscle, Fascia and Bone

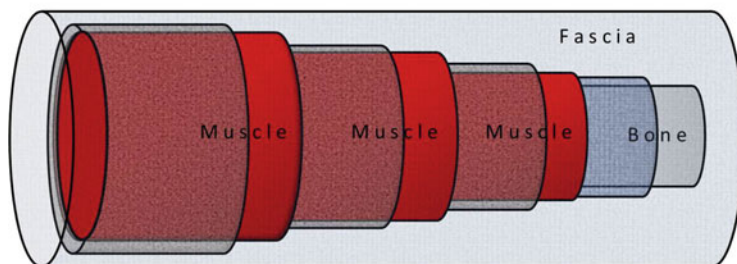


Fig. 2.2 Proposed topographic and biodynamic model for the human myofascial tension and support system comprised of bone with periost (inner semiluent tube), up to three skeletal muscle layers (red) with muscle fascia (lucent tubes), and the general fascia support of the muscle compartments (Fascia, overarching lucent tube). In this model, the bone structures represent force and strain-resistant support (by relative stiffness), the muscle layers represent actively contracting elements (tension and force production), and the various fascial structures represent passive viscoelastic support (tension and force storage) by connective tissue components, collagen fiber networks, and extracellular matrix molecules. The biomechanical properties (biomechanical stress response) of active and passive structures shown here may be affected in periods of disuse (unloading) and aging on Earth and during microgravity adaptation following long-term spaceflight

2.1.2 The Reinforcement Structures: Human Resting Myofascial Tension (HRMT) System and Entesis Organs (Including Tendons)

The contracting skeletal muscle (shortening of muscle) is the major force-producing component in human movement and performance probably representing one of the major vital expressions of life (e.g., contractile proteins → muscle → locomotion = > expression of life). However, a set of other nonmuscular connective tissue structural network always work in cooperation with normal muscle tension, contraction, and relaxation in order to adequately transmit the local biomechanical forces from the individual muscle fibers of a single muscle of a functional muscle group (extensors vs. flexors), for example, via muscle tendons inserted to the jointed bone levers throughout the human body to reinforce muscle contractions during various body motions in normal gravity (1G) on Earth. More recently, the structure and function of the various (almost forgotten) body fascia layers and, in particular, interface structures involved in biomechanical friction termed “enthese organs” (Benjamin et al. 2006) including tendons, myotendinous junctions (muscle-tendon interface), and osseotendinous junctions (tendon-bone interface), the retinacula of the knee and ankle joint, or even the flat tendinous structures known as aponeuroses that attach flat muscles to bone, for example, the great thoracolumbar fascia of the Latissimus dorsi back muscle, have been reconsidered as key biodynamical support structures of the human body. In addition, the dense regular and mesh-like connective tissue of a body-wide network of compression and tension (i.e., 3D tensegrity model of stiff and elastic structures) received more and more attention in the literature (Schleip et al. 2012). So far, the biomechanical roles of the body fascia under physiological and clinical aspects are only beginning to be reinvestigated as critical elements of an integrative body system termed the human resting myofascial tone and tension (HRMT) system (Masi et al. 2010).

The current view is that an estimated amount of about 10–30 % of total muscle power and force in the human body appears to be more or less stored by functional fascia and entheses related to the skeletal muscle system in normal everyday life or in exercise and sports (Huijing and Baan 2003). An altered structural composition of muscle or body fascia, for example, following longer periods of disuse or in the elderly may likely change the biomechanical properties (fascia may become either more flexible or stiff); however, very little is known about such adaptation mechanisms of the HRMT system in microgravity. As already routinely used in physical and rehabilitation medicine, physiotherapy, or osteopathy in practice, the term “myofascial tension system” should be used in addition to the term musculoskeletal system in the Human Space Life Sciences in order to underline its important structural and functional role for human performance control on Earth that were proposed to be further investigated in future ground-based analogues (bed rest disuse) and in human spaceflight (Lang T et al. Effect of long-duration spaceflight on bone and muscle: Report of the Bone-Muscle Expert Group, Cluster 1, Integrated

Systems Physiology, Theseus Project of ESA, European Science Foundation, and European Community's 7th Framework Program, FP7/2007–2013, unpublished).

In order to stimulate future research on the biomechanical properties of the various support systems of the musculoskeletal system, a comprehensive hypothetical biodynamic model for the human myofascial tension and support system is presented here that is based on functional anatomy and biodynamic properties of skeletal muscle, fascia, and bone and that is also used by the author in his academic teaching for second year medical students of the teaching module “Movement and Exercise” at the Charité Berlin, Germany (Fig. 2.2).

2.1.3 *The Little Power Chambers Inside: Sarcomere, Sarcoplasmic Reticulum (SR), and More*

A whole skeletal muscle is composed of larger and smaller bundles of skeletal myofibers (secondary and primary fascicles) mostly running throughout the length of a muscle and separated by perimysial connective tissue layers (Fig. 2.3). The secondary fascicles (sarcous fibers) are usually visible with the eye. In the microscope, a single muscle fiber is seen as a spindle-shaped elongated cell tube (about 20 cm in length, thickness comparable to a spiders thread, approx. 100 μm) closely packed with bundles of thin myofibrils composed of much thinner microfilaments

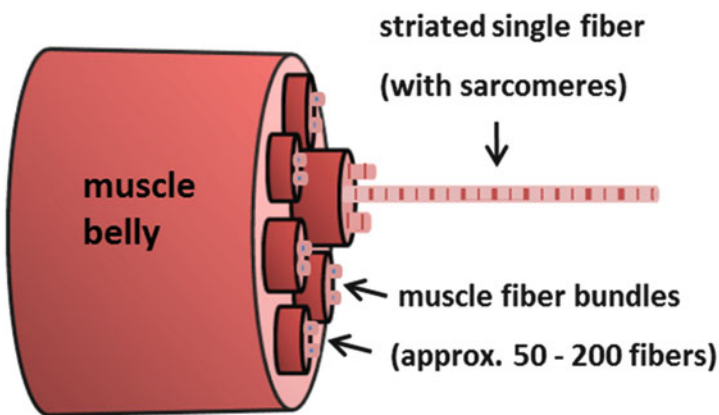


Fig. 2.3 A skeletal muscle (muscle belly) is ensheathed by a fascia and is composed of larger and smaller groups of fiber bundles (secondary and primary fascicles) embedded in loose connective tissue layers (perimysium) with neurovascular supply (capillaries, nerves, fibroblasts). A muscle fiber bundle contains approximately 50–200 striated individual fibers (polynucleated cell tube, sized 100 μm) embedded in a delicate connective tissue layer (endomysium). Each thin fiber is ensheathed by a basal lamina that provides mechanical support with extracellular matrix anchor molecules (laminin, fibronectin). Striated single muscle fibers contain bundles of myofibrils (1 μm) with their sarcomeres (little power chambers, sized 2–4 μm) in series (Fig. 2.4)

(thin actin, thick myosin filaments), with the calcium-dependent regulatory proteins (tropomyosin, troponin) responsible for actin-myosin interaction and the accessory proteins titin (spring-like protein) and nebulin (actomyosin stiffness) responsible for structural integrity, elasticity, and stiffness within the basic force-producing contractile component known as the sarcomere with its typical striated patterns (seen in light and electron microscopy) of A- and I-bands of overlapping actin-myosin microfilaments each anchored to the subtended Z-disks as the microstructural demarcations of a sarcomere (lat. *sarcos* = flesh) (Fig. 2.4, manuscript in preparation). Numerous sarcomeres (little power chambers) are arranged in series of about 500/mm of a

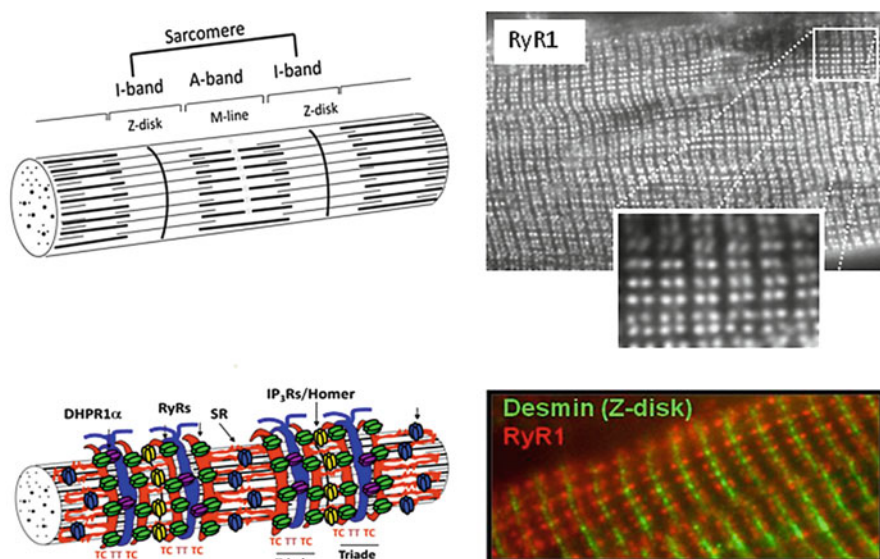


Fig. 2.4 Ultrastructural representation of a contractile sarcomere (serially power chamber) isolated from a myofibrillar bundle (*upper panel*) and its peri-sarcomeric support elements. As integral serial part of one long myofibril in a muscle fiber, the uncovered sarcomere structure has two adjacent endings (Z-disks) where the thin actin and thick myosin filaments are anchored and show overlapping regions. The main areas of thin actin microfilaments (*I-band*) and overlapping areas of thin actin and thick myosin microfilaments (*A-band*) are shown in the upper cartoon without support elements such as tubuli and other functional proteins. For better overview, the accessory sarcomeric filament proteins titin (filamentous spring-like stabilizers that span throughout the sarcomere from the adjacent Z-disks) and nebulin (connectivity functions during actin-myosin interactions) are not shown (*lower panel, left*). The sarcomeres are surrounded (covered) by tubular networks of the sarcoplasmic reticulum structures (SR) of the longitudinal system (L-tubuli, *thin red lines*) with terminal cisterns (TC, *thick red semicircles*) and transverse tubules (TT, *thick blue semicircles*) which are membrane extensions of the outer membrane into the muscle fiber. The main typical SR-associated calcium channel proteins are shown by four subunit protein icons of various colors, RyR1 (*green*), SERCA (*blue*), DHPR (*purple*), and IP₃R/Homer (*yellow*). Another protein called Homer is located adjacent to Z-disk structures but also at the subsynaptic microdomain (not shown, see Chap. 3.0). *Lower panel (right)* shows double staining by immunohistochemistry with anti-desmin (Z-disk marker, *green*) and anti-RyR1 (*red*) antibodies in two or three adjacent striated rat muscle fibers (Manuscript in preparation)

muscle fiber so that the microscopic shortenings of individual sarcomeres add up to the visible muscle contractions and macroscopic changes in muscle length, for example, during body motions. Skeletal muscle fibers contain all the typical cell organelles found in any other nucleated cell type (mitochondria, Golgi apparatus, endoplasmic reticulum, vesicles), but, unlike most single-nucleated cell types of the body, they contain about a hundred of myonuclei for gene transcriptional control of subcellularly partitioned microdomains for normal cell metabolism and adaptation. Muscle fibers also contain a complex and specialized endoplasmic network of tubules known as the sarcoplasmic reticulum (SR) that express a set of calcium release and calcium uptake proteins (ryanodine receptor, SERCA) which actively transport calcium ions from this major calcium store to the sarcosol and vice versa (influx/efflux) to enable normal fiber contraction during excitation. For more details, refer to a current book chapter by Brenner and Maasen (2013) and shown in this chapter (Fig. 2.18).

2.1.4 Muscle Works Against Gravitational Forces on Earth

In order to cushion the gravitational load forces, movements of the human body are biodynamically controlled via muscle by muscle contraction in accordance with a typical pattern known as “closed muscle chains” (e.g., activated in squat down by knee bending). In “open muscle chain” movements, for example, arms or legs are freely moved away from the body axis however against gravitational load but in absence of whole body weight loading (e.g., lifting of the arms or of one leg only during standing or recumbent body position). A more detailed description of the human skeletal muscle system based on topographical and functional muscle compartments is found in a current book chapter elsewhere (Blottner 2013).

In microgravity, movements of the floating human body are mainly performed according to the open muscle chain type due to gravitational unloading. However, gravitational loading can be simulated during inflight exercise by pressing the body with elastic straps fixed to comfortable body harnesses (shoulder and hip) to a fixed point of an exercise device during the training bouts, thus simulating closed muscle chain movements at least under partial resistance loading conditions in spaceflight (see Sect. 2.1.1 and next chapters).

2.1.5 Current Definitions of Human Skeletal Muscle Contraction Types Under Normal Gravity Conditions on Earth (1G)

Dynamic skeletal muscle is attached to relatively stable or stiff bone (point of origin) via more flexible osseotendinous junctions (muscle-tendon-bone) and

further runs over joints to their points of insertion on another bone (usually distal to the same joint). The main function of skeletal muscle is contraction (shortening) which brings the two bones (lever arms) closer together to initiate active mode body motions during voluntary movements. This type of a “visible” muscle activity is usually considered by most people as a muscle contraction with force production. In passive mode body motions, however, muscles are passively moved (i.e., they are shortened or slightly stretched) against gravitational load (i.e., passive arm or leg movements without voluntary forces) usually performed without one’s own muscle force, however, with the help of the force of a therapist (Sect. 2.2.1.1). The muscle in action is termed the agonist (e.g., biceps brachii during arm bending), while its counterpart is termed the antagonist (e.g., triceps brachii during arm bending). In this example, active and passive stretching of skeletal muscle is performed alternately between agonist and antagonist contractions during normal elbow joint movements.

The basic muscular contractions include **isotonic contraction** (muscle shortens in length under constant work/tension against gravity, e.g., arm lifting a heavy book from table for reading, maximal force is larger than the gravitational load of an object), **isometric contraction** (muscle remains the same length under constant work/tension against gravity, e.g., holding a heavy book in front of the body or carrying a heavy bag, the muscle force precisely matches the gravitational load), and **auxotonic contraction** (simultaneous change in length and force under constant work against gravity, e.g., heavy weight lifters, muscle force becomes higher during lifting motions). In addition, stopped preloaded contractions (e.g., masticatory pressure following teeth occlusion) and afterload contractions (e.g., lifting an object with changed effective lever arms) are composite types of contractions including isotonic, isometric, and auxotonic contractions (Brenner and Maasen 2013).

In muscle exercise, muscular strength (force) is usually increased by resistance (resistive) training which is a combination between concentric (shortening contraction, force generated while shortening occurs sufficient to overcome gravitational load) and eccentric muscle loading (lengthening contraction, force generated while muscle elongates under tension such as during deceleration of an object or lowering an object gently, the force generated becomes more and more insufficient to overcome gravitational load). Eccentric muscle contraction is typically performed during sit-ups, squatting exercises, or arm press-ups (body weight load) or with additional loading using barbells, dumbbells, or elastic straps in normal fitness or extensive strength training protocols. Compared to concentric loading, heavy eccentric loading (muscle building, strength training) has some considerable risk of muscle damage (Faulkner 2003).

2.1.6 Histologic and Molecular Adaptation in Normal, Atrophic, and Gravitational Unloaded Skeletal Muscle

Normal human skeletal muscle consists of various types of muscles with predominantly slow (type I, e.g., soleus) and predominantly fast myofiber-type (type II, e.g., brachioradialis) distribution patterns, and a variable number of muscles with mixed slow/fast fiber types (e.g., vastus lateralis) currently reviewed (Blauww et al. 2013; Schiaffino and Reggiani 2011). The normal human vastus lateralis (Fig. 2.5) of younger males (17–33 years of age, Johnson et al. 1973) consists of a mixture of fast-twitch (type II) and slow-twitch (type I) myofibers in a varying composition (approximately 65 % fast vs. 35 % slow fibers), while the antigravity calf muscle, the soleus, mainly consists of slow-type myofibers (approx. 85 % slow vs. 15 % fast). If isoform-specific MyHC subtype markers are used as detectable immunomarkers during human skeletal muscle adaptation, variable numbers of fast myofiber subtypes (IIa, IIx) are usually found, while the IIb fiber subtypes are only found in a few defined human skeletal muscle species (e.g., extraocular, pharyngeal, laryngeal). The MyHC IIb subtypes are, however, frequently found in rat or mice skeletal muscle (Ciciliot et al. 2013).

In addition to the size and phenotype distribution changes observed in disuse, the integrity of the outer muscle fiber membrane (sarcolemma) and the subsarcolemmal dystrophin scaffold structures are also compromised in human and animal skeletal muscle disuse. The dystrophin proteins are considered as key proteins of the muscle fiber subsarcolemmal scaffold helping in membrane stabilization and membrane-actin stiffness (Sarkis et al. 2013). In our work, we showed that the subsarcolemmal localized protein dystrophin also serves as a valuable immunohistochemical marker

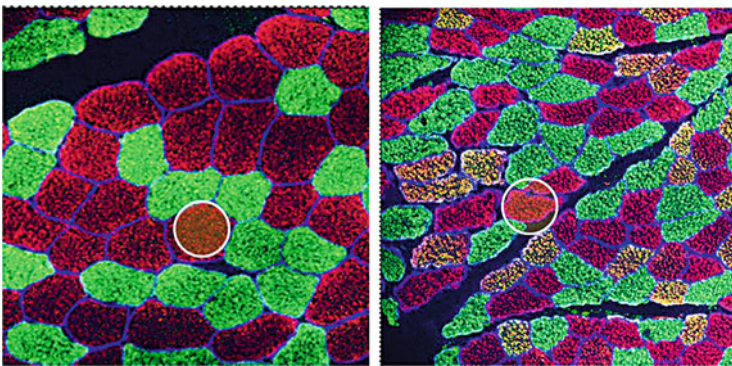


Fig. 2.5 Myofiber-type distribution (mixed 60:40 % fast type 2a,x vs. slow type 1) and cross-sectional area (CSA) size changes in normal (*left*) versus atrophic (*right*) human vastus lateralis (VL) after 60 days of disuse in bed rest (BBR-1 study, Charité Berlin). Slow type 1 (*green*), fast type 2a/x (*red*), and hybrid (*yellow*) myofibers expressing both slow and fast myosin heavy chain (s/fMyHC) immunolabels as a sign of disuse-induced fiber slow-to-fast transition. In both images, the myofiber CSA size change is marked in two cross-sectioned myofiber profiles by a white circle (approx. 4,000 μm^2) of identical area

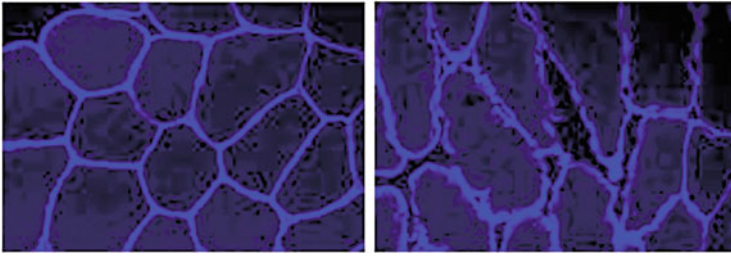


Fig. 2.6 Dystrophin immunohistochemical patterns in cross-sectioned myofibers of a normal (*left*) and chronically disused (*right*) human vastus lateralis (VL) reflecting disuse-induced sarcolemmal disintegration in long-term bed rest (60 days BBR-2 study, Charité Berlin, 2007)

to show altered membrane integrity patterns in normal versus disused human skeletal muscle in cryosections following prolonged disuse in bed rest (Salanova et al. 2014; Blottner et al. [in press](#)). The dystrophin immunolabel has been routinely implemented to our immunohistochemical protocols for many years now to clearly identify the outer demarcations of muscle fibers to improve qualitative and quantitative analysis of skeletal muscle fiber structures and biochemical properties on biopsy cryosections in normal versus disused human skeletal muscle as well as in space-related animal studies (Fig. 2.6).

In skeletal muscle atrophy, a fiber-type specificity exists for the regulation of muscle mass. For example, fast glycolytic fibers (type II) are more vulnerable than slow oxidative fibers (type I) that correlated with distinct signaling pathways, for example, signaling transduction of forkhead box-O family transcription factors (FOXO), autophagy inhibition, transforming growth factor-beta (TGF- β family), and nuclear factor-kappa- β (NF- κ B) expression (Wang and Pessin 2013). The resistance of oxidative fibers to atrophy may be explained by the protective mechanisms elicited by peroxisome proliferator-activated receptor gamma coactivator 1-alpha, PGC1 α (Olesen et al. 2010; Wang and Pessin 2013). A number of current reviews are available on the mechanisms modulating the muscle phenotype based on slow versus fast myofiber fiber patterns (Blaauw et al. 2013), on the molecular basis of muscle atrophy including the IGF/Akt/mTOR pathway and the myostatin/Smad pathways, on the non-lysosomal ubiquitin proteasome pathway of muscle protein degradation via the E3 ligase proteins MuRF1/Mafbx/atrogenin-1 (Jackman and Kandarian 2004; Murton et al. 2008; Bodine-Fowler et al. 1995; Bodine and Baar 2012), on the countermeasure impact on signaling pathways in disuse (Chopard et al. 2009), and on nutritional aspects and the still controversially discussed muscle protein accretion/wasting mechanisms (e.g., protein synthesis vs. breakdown) in disuse atrophy and the impact of nutrient supplementation against imbalanced muscle protein turnover in disuse (Stein and Blanc 2011) (Fig. 2.7).

Skeletal muscle disuse normally shows a slow-to-fast fiber shift likely controlled by PGC1 α expression and related signal pathways upregulated by exercise (Olesen et al. 2010; Handschin 2010; Peterson et al. 2011) likely affected by physical

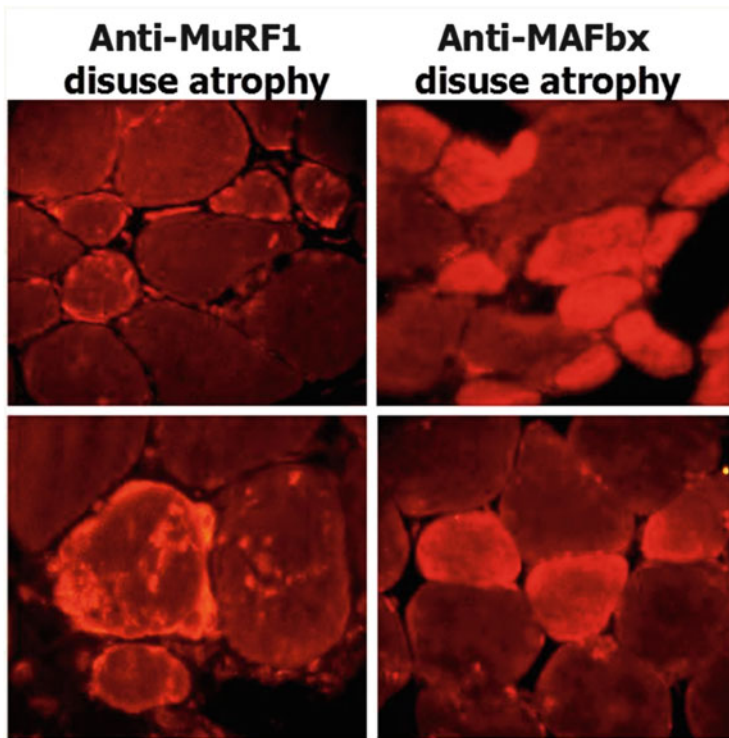


Fig. 2.7 MuRF1/MAFbx immunostaining (*red*) in cross-sectioned myofibers of disused normal human skeletal muscle fibers in female bed rest (2003 WISE-Study, Toulouse, France). Both immunolabels were used to visualize protein degradation (proteolysis) at the myofiber level following disuse (Courtesy: B. Schoser, LMU Munich (Salanova et al. 2008))

exercise as countermeasure (Desplanches 1997). An increased amount of hybrid fibers (co-expressing the slow and fast fiber phenotype, in the range of $5 < 15\%$) compared to normal ($2 < 5\%$ baseline) found in various atrophy models by slow/fast myosin heavy chain (MyHC) immunohistochemistry, immunoblotting, and proteomic analysis are considered as signs of fiber-type-related transient shifting and remodeling mechanisms in various muscle disuse paradigms without and with exercise as countermeasure (Salanova et al. 2008; Salanova et al. 2009b; Moriggi et al. 2010; Luxa et al. 2013; Sun et al. 2013).

The loss in muscle mass and the basic structural and functional consequences of unloading/disuse atrophy for skeletal muscle are well described (LeBlanc et al. 1992; Fitts et al. 2001). For example, in atrophic fibers following disuse/unloading, the fiber cross-sectional area (FCSA) and the myonuclear numbers are diminished (Ohira et al. 2002), and the fiber-type distribution in a given unloaded muscle shifts from slow to fast (fiber shift or transition) resulting in reduced force-generating capacity. In gravitational unloading in animals (HU-rats), the percentage of fibers expressing fast MyHC isoforms increases in unloaded soleus but not in fast

muscles suggesting that predominantly slow muscles are more responsive to gravitational unloading than predominantly fast muscles (Ohira et al. 2002).

Even if extremely useful as a ground-based spaceflight analogue (Booth 1994), disuse in bed rest may be an extreme model of physical inactivity (Thyfault and Booth 2011), for example, to investigate the changes following sedentary lifestyles or even aging of modern societies. However, bed rest immobilization appears to also mimic many of the structural and functional changes observed in sedentary lifestyle residents (loss in muscle mass and force, others) either challenged by extended sitting time or much to low daily stepping patterns (<3,000 steps/day/healthy adults) compared to a physically active lifestyle with approximately > 7,000 steps/day of a recommended physical activity (Tudor-Locke et al. 2011).

However, the actual fiber composition in a normal healthy skeletal muscle largely depends on genetic predispositions and may vary due to lifestyle, history of activity, and sex and age of a subject (Baldwin and Haddad 2002). After analyzing more than 800 muscle biopsies from mainly slow and slow-/fast-mixed muscle types of healthy human subjects over the last decade, we suggest that apart from the known intersubject variability and sex differences, for example, between male and female muscle, a continuum of the myofiber-type distribution should be considered because of ongoing adaptation processes throughout normal human life on Earth. In laboratory rats and mice of comparable genetic strains, the muscle fiber size and type changes are “more stable” due to controlled housing conditions in standard vivarium cages (IVC cage) with defined group sizes, activity status, and feeding of standardized nutrients. Even smaller cages (<50 % reduced floor area vs. IVC cages) may not confound structural biochemical and behavioral analysis of laboratory mice (C57Bl/6 strain) even under fully automated life support housing conditions usually required for rodent spaceflight experiments (Blottner et al. 2009).

Due to the relatively well-known fiber-type composition of human skeletal muscle and due to their well-palpable anatomical location in the human body, two of them, the vastus lateralis and the soleus, have been considered by many laboratories around the world as standard reference muscles for the reliable statistical analysis in previous bed rest studies and most probably also in crew members for comparability reasons of ground and flight sample analysis.

2.1.7 NO Signals in Muscle: Nitric Oxide (NO) Produced by NO-Synthase (NOS) as Multifunctional Signals in Normal Muscle Physiology

With the discovery of nitric oxide (NO), formerly known as endothelial-derived relaxation factor (EDRF), biological gas signals were of particular interest in fundamental muscle biology and physiology (Bredt and Snyder 1990), disease (Brenman et al. 1995), clinical applications (Zhou and Zhu 2009), and, more recently,

also in sports and exercise biology (Suhr et al. 2013). Biological NO signals were described in the late 1980s (around 1987–1989) as a completely new class of diffusible gaseous signals first described in vascular endothelial cells (NO as vasodilator) and in subsets of neuronal cells (NO as diffusible neurotransmitter, long-term potentiation) of the brain by several scientists including Salvador Moncada from the UK, but also by the US scientists Louis Ignarro, Ferid Murad, and Robert Furchtgott (Nobel Prize in physiology and medicine in 1998). In addition to NO signals found in the vasculature (endothelial NOS, eNOS) and central and peripheral neuronal networks (neuronal NOS, nNOS), skeletal muscle soon was identified as another large source of NO signals in the body (Nakane et al. 1993; Silvagno et al. 1996) including ventilatory muscles (Hussain et al. 1997). The skeletal muscle-derived NO signals and their dynamic roles in contraction and force mechanisms, myocellular metabolism, and cell signaling pathways became of particular interest for skeletal muscle biology and various adaptation mechanisms related to muscle structure and physiology. Currently, at least three individual NO-synthase genes are known, termed NOS1 (nNOS, neuronal), NOS2 (iNOS, inducible), and NOS3 (eNOS, endothelial) according to the proposed new terminology for NOS isoforms (Stamler and Meissner 2001) with about 20 different splice variants (Brenman et al. 1997) (Fig. 2.8). A muscle-specific splice variant of NOS1, termed m μ NOS (Silvagno et al. 1996), was characterized as part of the dystrophin-glycoprotein complex of the skeletal muscle fiber membrane (sarcolemma) where m μ NOS/NOS1 is anchored through a PDZ motif at its NH₂ terminus to alpha and beta syntrophins and thus to dystrophin and dystrobrevin (Grozdanovic and Baumgarten 1999; Percival et al. 2008).

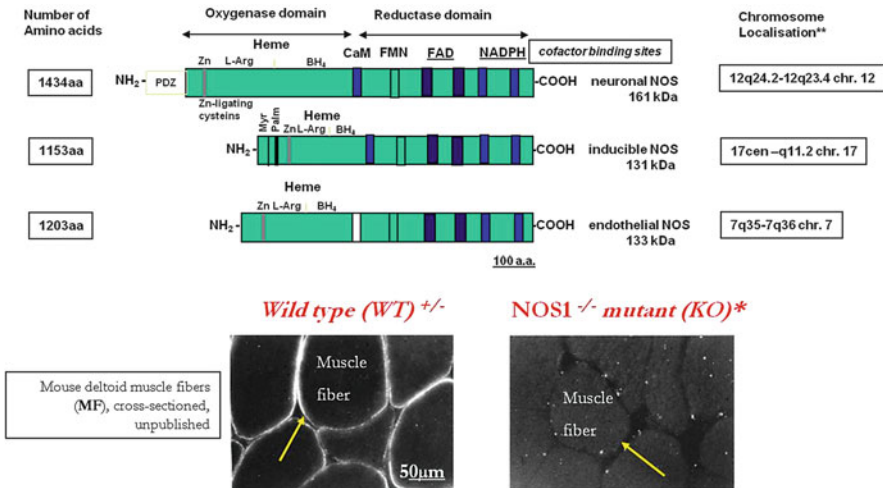


Fig. 2.8 Domain structure of NOS 1–3 genes on three human chromosomes. Skeletal muscle sarcolemmal nNOS immunolocalization (arrows) in wild-type versus nNOS^{−/−} mutant mice deltoid muscle fibers (cross sections), D. Blottner, unpublished. Cartoon (upper panel) mod. from Ignarro LJ (ed) Nitric oxide biology and pathobiology, Academic Press, p.12 (2000)

NO signals are considered as metabolic regulators during muscle exercise in health and disease (Kingwell 2000) but also during muscle denervation and reinnervation (Tews et al. 1997; Rubinstein et al. 1998) and in muscle repair and remodeling mechanisms via satellite cells (Anderson 2000). Imbalance in NO signal mechanisms results in movement impairments such as slowing the walking speed in rats following *in vivo* NOS inhibition (Wang et al. 2001). Our previous basic research on the muscular NOS/NO system aimed at investigating the spatio-temporal expression and localization patterns using immunofluorescence methods with isoform-specific NOS antibodies in conjunction with nonradioactive NOS mRNA *in situ* hybridization techniques in skeletal muscle development that showed that all three major NOS1-3 isoforms are basically expressed in mouse C2C12 single myoblasts that are transiently upregulated when the single-nucleated myoblast fusion to become elongated multinucleated myotubes *in vitro* that eventually differentiate into mature skeletal muscle fibers (Blottner et al. 1998). Other work showed that explanted single muscle fibers are able to release measureable NO signals into the culture medium upon *in vitro* drug administration (NO-donors, arginine, or nitroprusside, Balon and Nadler 1994) and following *in vivo* electrical stimulation in the rabbit possibly involved in metabolic control of fiber phenotype transformation of anterior tibialis and extensor digitorum muscle (Reiser et al. 1997). In addition, mechanical loading was found to affect NOS expression by *in vitro* (myotubes) and *in vivo* (HU-rat) experiments confirming activity-dependent muscular NO signaling (Tidball et al. 1998; Fujii et al. 1998). Other studies in adult animals found that the sarcolemmal NOS is able to translocate from membrane to the sarcosol (cytosol) in response to mechanical unloading (Suzuki et al. 2007). Interestingly, the NOS2 isoform (inducible NOS) was found to be associated with the outer membrane protein caveolin-3 in slow-twitch guinea pig muscle suggesting involvement, for example, in glucose metabolism (Gath et al. 1999), a finding that was confirmed by our group in normal human muscle by altered NOS2-caveolin-3 co-expression following bed rest (Rudnick et al. 2004). In cultured C2 myotubes (mouse C2 cell line), we showed that NOS1 proteins co-cluster together with nicotinic acetylcholine receptors (major component of cholinergic synapses) by agrin-induced postsynaptic membrane clusters *in vitro* (Lück et al. 2000; Blottner and Lück 2001), and upon motor nerve contacting, the myocellular NO signals were upregulated in C2 myotubes in nerve-muscle cocultures performed in our laboratory (Püttmann et al. 2005). Nitric oxide synthase is expressed at the adult neuromuscular synapse (Kusner and Kaminski 1996) during development suggesting multiple signaling functions for neural transmission from motor nerve to skeletal muscle fiber (Blottner and Lück 2001). These studies showed that muscular NO signals are apparently regulated by neuronal mechanisms and should therefore have crucial signaling functions in postsynaptic neuromuscular control of skeletal muscle (Oliver et al. 1996).

Earlier work from our laboratory also suggested a sarcolemmal NOS1 localization as shown by NOS immunohistochemistry and also by the NADPH diaphorase enzyme histochemical activity (histochemical marker of NOS activity) in developing rat and mouse normal skeletal muscle by our group (Blottner and Lück 1998;

Lück et al. 1998). In those studies, we found a gradient of increased sarcolemmal NOS expression in developing mice muscle fibers before and around birth (perinatally). In further animal and human studies, investigations on the muscular NOS/NO system turned out to serve as a valuable biomarker to study disuse atrophy (loss and/or translocation of myocellular NOS) and to assess efficacy of exercise countermeasure (preservation of myocellular NOS) in bed rest (see Sect. 2.2.3.4).

2.2 Lessons Learned from Ground-Based and Spaceflight Experiments

2.2.1 *Animal Studies on Earth*

Up to now, established and current in vitro models use isolated cells and tissues and multipotent stem cells cultivated in defined nutrient solutions under controlled conditions in special laboratory incubators. They are useful tools to study fundamental mechanisms in cell biology and physiology including cell development, differentiation, and growth, for example, triggered by bioactive molecules (growth factors, cytokines) by pharmacological in vitro cell assays as standard methods routinely used in research laboratories around the world. In gravitational and radiation biology, isolated primary cells, cell lines, or tissues are used to study microgravity changes in plant and animal cell biology grown in special cell incubators as payload to study fundamental mechanisms “unmasked of gravity” (Unsworth and Lelkes 1998), for example, cell shape and cytoskeleton changes in gravisensing (Hughes-Fulford 2003), bone cell signaling (Hughes-Fulford 2004), and cartilage differentiation (Duke and Montufar-Solis 1999), just to mention some of the cell biology experiments already flown in Space.

Skeletal muscle research offers a battery of myogenic cells (myoblasts, myotubes), isolated muscle fibers, and muscular stem cells (satellite cells) that are currently available to study defined aspects of physiological and pathophysiological mechanisms (e.g., fiber contractility, muscle development, and regeneration on Earth (Aas et al. 2013) as well as in simulated microgravity (Benavides Damm et al. 2013) and in spaceflight experiments (Franzoso et al. 2009).

However, isolated single cells or cell layers from various tissues sources (bone, muscle, brain, others) may not fully replace in vivo studies in small laboratory animals (rats and mice) as, for example, currently demonstrated by a successful stem cell therapy (stem cells were cultivated in vitro and afterward implanted in vivo) to offset skeletal muscle atrophy in mice (Artioli et al. 2014).

In vivo studies are essential to further understand the complexity of integrative signaling processes and their adaptation mechanisms inherent to the neuromuscular system in a normal living higher vertebrate organism including also humans. Due to cost limitations and other spaceflight constraints (design of animal housing devices for spaceflight), most of the animal studies in space research are performed by

international scientific laboratories on the ground with expert staff and adequate equipment in animal facilities according to commonly accepted regulations for use and care of animals in scientific research consented and approved by national and local ethical board members of various disciplines (NRC 1996; Katahira 2001).

2.2.1.1 Ground-Based Experiments I: Hind Limb Unloading (HU) in Rats

Hind-limb unloading (HU) of the rat is a traditional and well-established ground-based experimental animal research paradigm in spaceflight research used by NASA to study disuse atrophy in small rodents such as rats (Morey-Holton and Globus 2002) or mice (Ferreira et al. 2011). Experiments with the HU-rat model require specially designed cages as animals need to move freely with both fore paws touching the ground for water and food ad libitum while the rat's body is in a 30° angle to secure for hind-limb unloading (HU position, i.e., tail suspension) with both hind limbs freely hanging down without touching the bottom of the cage. Due to the common regulations of animal use and care in research, only laboratories with specialized animal facilities are able to use rats or mice over several days or weeks for HU experiments (Morey-Holton and Globus 2002). Because of ethical reasons, HU animal studies should be performed in cooperation between laboratories for optimal tissue sharing and analysis (Morey-Holton et al. 2007).

In a bilateral and interdisciplinary university cooperative between the Charité Berlin, Germany, and the Beihang University Beijing, China, we were able to share muscle tissue from a rat 21d HU experiment performed with a custom-made stepper device for rodents by our Chinese partners from the Key Laboratory of Biomechanics and Mechanobiology at the Beihang University to study bone and muscle loss under active versus passive muscle training (Sun et al. 2013). We found that the NOS1 biomarker in HU-rat soleus muscle almost disappeared from the unloaded myofiber sarcolemma (after 21 days of HU) compared to control animals (vivarium control). This loss in sarcolemmal NOS 1 was, however, prevented by active stepper training of hind limbs during HU position (reflexive muscle contractions triggered by plantar electric pulse arc stimulation) and to lesser extent also by passive stepper training during HU (passive mode motions induced by up and down movements of hind legs during HU via motorized foot pedals) compared to relevant controls performing comparable stepper training in normal body position in vivarium standard cages (Sun et al. 2013). This direct comparison between active and passive motions of disused rat skeletal muscle can be experimentally investigated only by the HU protocol that provided conclusive evidence for the presence of an activity-driven sarcolemmal NOS1 translocation from the myofiber sarcolemma to the sarcosol that can be offset by adequate muscle training (Sun et al. 2013). The results are interesting because activity-driven NO signals control a set of functional muscle-specific proteins via protein-S-nitrosylation, and, for example, abundant NO signals (too much or too little) could explain some of the altered muscular functions observed in human skeletal muscle disuse by nitrosative stress mechanisms

experimentally proven in bed rest by our laboratory (see Sect. 2.2.3.5). In the same HU experiment, active stepping of gravitationally unloaded rat hind limbs prevented loss in tibial bone mass (the soleus originates from to the tibia) and trabecular microarchitecture, supporting the notion for optimization of human countermeasure protocols that should be targeted to individual human muscle-bone units following disuse on Earth, in rehabilitation, or in spaceflight.

2.2.1.2 Ground-Based Experiments II: Vestibular Deafferentation in Rats

As already discussed in the introduction chapter, the vestibular system (organ of equilibrium) is a key equilibrium and spatial reference system for adequate body movement control on Earth that undergoes considerable modifications during spaceflight with obvious consequences on spatial orientation and well-being in crew members who, for example, may suffer from space motion sickness (Lackner and Dizio 2006). Previous findings from the literature suggested that the vestibular outflow may control general sympathetic outflow in the body and, in particular, also the muscular sympathetic nerve activity on Earth as well as in Space. For example, baseline sympathetic outflow was found to be increased as a reason for hemodynamic stress in humans in Space (Eckberg et al. 2003); human sympathetic nerve activity is reduced after short microgravity exposition (parabolic flight) and upregulated after longer periods of microgravity (spaceflight) with impaired arterial baroreflex (Mano and Iwase 2003; Mano 2005) concomitant to altered human muscle sympathetic nerve activity (Ertl et al. 2002). However, the obvious role of vestibular changes for skeletal muscle disuse atrophy received only little attention (Kasri et al. 2004; Tothova et al. 2006).

In a laboratory cooperation between the Physiology Department at the University of Caen, France, and the Neuromuscular Group at the Charité Berlin, we tested the hypothesis that the vestibular system may affect both myofiber size and type composition of skeletal muscle in normal adult rats ($n = 8$) subjected to vestibular deafferentation (labyrinthectomy) in a 30-day long laboratory experiment established by our French partner laboratory. This experiment made use of surgical removal of the vestibular system in rats or mice to extinct the gravity stimulus by destruction of the gravisensor on Earth (Jamon 2014). Compared to sham-treated controls (with still intact gravisensors), *in vivo* bilaterally vestibular lesioned rats now missing the graviceptors showed significant myofiber size reductions in tissue samples of postural soleus muscle, altered fiber-type composition, and reduced myonuclear NFATc1 transcription factor accumulation (i.e., NFATc1 shift from cytosol to nucleus), all signs of slow myofiber atrophy remodeling and transcriptional activity changes in slow myofibers of postural soleus muscle (Luxa et al. 2013). Interestingly, vestibular lesions also resulted in considerable bone loss in this animal model (Denise et al. 2009) with clinical implications considering the identification of a unique inner ear signal control of bone formation (Vignaux et al. 2013) and possibly also acting on skeletal muscle quality (Luxa et al. 2013).

Even if the exact neuroanatomical links remain to be elucidated, it seems likely that, similar to bone formation, skeletal muscle adaptation may be controlled by autonomic nervous system signals via spinal vestibul sympathetic outflow to peripheral targets to support normal skeletal muscle mass and function under terrestrial gravity (Luxa et al. 2013). These findings are of particular interest to find more adequate countermeasures against microgravity-induced muscle atrophy and bone loss for the crew members in future spaceflights. These findings also may have some impact on the clinical management of common vestibul sympathetic disorders (Ménière's disease), for example, for better interpretation of clinically feasible skeletal muscle monitoring by vestibular evoked myogenic potentials to reliably determine inner ear vestibular saccule function (Honaker and Samy 2007).

2.2.2 *Animal Studies in Spaceflight*

Since the early days of spaceflight, animals were frequently flown in Space by NASA and the Russian Space Agencies onboard satellites on orbit (Cosmos) for several days up to a few weeks (Morey-Holton et al. 2007; Ballard and Rossberg Walker 1992; Oganov et al. 2006). A review on the history of spaceflown animals “from the first dog to the last monkey in space” can be found elsewhere (Ilyin 2007). Animal experiments in space with higher vertebrates and mammals are essential to study the physiological mechanisms working in the human body in microgravity (Yamasaki and Shimizu 2004) in sufficient statistical numbers. Our group participated to an international muscle team involved in two flight experiments with rodents in Space, one in 2009 (MDS mission, Sect. 2.2.2.1) with mice housed for over 90 days in a special animal payload on the ISS (mice drawer system, MDS, 2009), supported by the Italian Space Agency (ASI), NASA, and JAXA, and another one in 2013 with adult mice flown on a Russian biosatellite (BION-M1, Sect. 2.2.2.2), supported by the DLR (Germany) and IMBP (Russia).

It should be noted that mice are housed in Space in smaller cages (reduced area cages) than normally used in animal vivarium on the ground (standard ICV cages) with the potential risk of confounding results obtained by spaceflight experiments with mice living on reduced area (floor size) with, for example, less activity levels and challenged by higher stress levels (noninvasively analyzed by corticosteroid monitoring of feces). However, pilot laboratory experiments with C57/Bl6 mice housed in automated life support cages with reduced floor areas (MRSM cages, Fig. 2.9) for 3 weeks at the laboratory of our cooperation partners of the Measure, Model, and Manage Bio-Responses (M3-BIORES) working group at the University of Leuven (Kastelpark Arenberg, Heverlee), Belgium, revealed little if any negative effects on musculoskeletal system and behavioral outcome (stress and learning) produced by the unique cage design (Fig. 2.9) suggesting that the new environmental condition may not confound structure, physiology, and behavior results from Space Life Sciences research experiments and suggesting that mice pre-adapted to fully automated life support animal habitats for about 1 week prior to



Fig. 2.9 Ground-based mouse science reference module (MRSM) experiment performed together with an ESA/ASI supported multidisciplinary MISS Facility Science Team (FST) of scientific experts (L. Vico, M. Jamon, D. Berckmans, D. Blottner), ESA representatives (P. Schiller, O. Angerer, J. Hatton, F. Gaubert), ASI representatives (V. Cotronei), and industrial partners from Thales-Alenia Space (G. Falcetti) located at the Catholic University of Leuven, Belgium, in 2006–2007. Biological testing was performed for any structural, physiological, and behavioral parameter changes of male C57Bl/6 mice housed (singly or in pairs) in small animal habitats (cf. three reduced floor size cages seen in middle racks) compared to standard-sized IVC cages integrated in the same rack shown (at the right side). Each mice habitat (cage) has an automated food supply system on its rear wall, a waste filter system underneath the cage bottom. Cages are air-conditioned through a closed tube system connected to an automated life support system (not shown) for ambient air ventilation, temperature, and humidity control (Blottner et al. 2009)

launch (astromice) should be implemented in future scenarios of spaceflight experiments (Blottner et al. 2009).

2.2.2.1 Mice on the International Space Station (ISS). MDS Mission

In 2009, a spaceflight payload for rodent research on the ISS, the mice drawer system (MDS), was initiated by the Italian Space Agency (ASI) and designed by Thales Alenia Space Italia company (Fig. 2.10). The MDS payload was flown to the ISS via the Shuttle Discovery 17A/STS-128 (Aug 28th, 2009) and returned to Earth with Shuttle Atlantis ULF3/STS-129 (Nov 27th) after 91 days in Space, which currently still is the longest permanence of mice in Space ever (Cancedda et al. 2012). The MDS housed six mice (3 wild-type and 3 PTN-Tg mutant mice, overexpressing a bone-specific promoter for pleiotropin (Fig. 2.10). Unfortunately, three mice died during the MDS mission due to health status and payload-related reasons. The remaining mice showed a normal behavior during the experiment, food and water and health status were daily checked, and they appeared in excellent

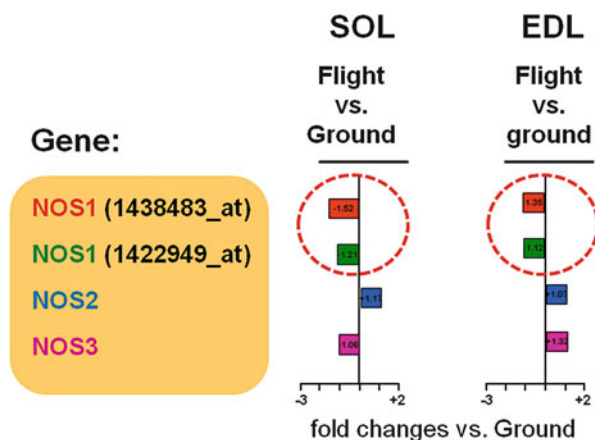


Fig. 2.10 The 91 days duration mice drawer system (MDS) module scenario (Aug 28 to Nov 27, 2009, STS 128/129, PI Cancedda) on the International Space Station (ISS). NASA Astronaut Nicole Scott onboard the ISS at the Japanese Kibo Laboratory with the MDS module (right side) housing three ($n = 3$) C57Bl/10 J and three ($n = 3$) *osf-1* transgenic mice (Courtesy: NASA (<http://onorbit.com/node/1601>))

health after landing. To receive as much information as possible on the microgravity-induced changes, spaceflown mice were immediately sacrificed upon return from Space, the various tissues of interest dissected within 24 h after landing and distributed to a Tissue Sharing Team of about 20 research teams from 6 countries including Germany (Charité Berlin). A ground replica of the flight experiment including animal housing in a second ground-based MDS drawer device was performed in parallel to the spaceflight experiment in the PI's laboratory (R. Cancedda) of the University of Genova, Italy. In addition, control tissue was also obtained from mice housed in standard vivarium cages on Earth (Cancedda et al. 2012).

The skeletal muscle changes of the MDS mice include a slow-to-fast transition of the soleus myofibers (type 1/type 2 shift) and slow/fast myosin heavy chain content typically for this postural muscle following extended microgravity unloading. The sarcolemmal NOS1 translocation to the sarcosol was also found after prolonged microgravity exposure (Sandona et al. 2012) as well as flight-related NOS1–3 gene expression in a muscle-specific pattern (SOL vs. EDL) by microarray analysis (Fig. 2.11) confirming the previous ground-based experimental results reported by our group exposed to simulated microgravity models in animals (HU) and humans (bed rest). Moreover, a set of atrophy-related ubiquitin ligases (MuRF E3 ligase), sarcolemmal ion channels (NAV1.4, K⁺ –channel subunits Kir6.2, SUR2A, and SUR1), various stress-related genes (NF- κ B), and transcription factors (MRF-4) were upregulated in spaceflown soleus muscle compared to ground

Fig. 2.11 Nitric oxide synthase isoform (NOS1-3) gene expression (microarrays) in mouse soleus (*SOL*) and extensor digitorum (*EDL*) skeletal muscle following long-term spaceflight (flight) onboard the ISS (91d MDS mission) compared to ground controls (ground) (Manuscript in preparation)



controls (Sandona et al. 2012). In conclusion, antigravity muscles such as the soleus react in a very sensitive way against prolonged microgravity exposure, while other calf muscles (EDL) were more resistant to unloading probably by activating compensatory and protective signaling pathways. These results support the idea to identify molecular targets for the new development of countermeasures (Sandona et al. 2012). Some of the results of the MDS mission, for example, on bone, muscle, and brain of the spaceflown mice including our data on skeletal muscle, are published elsewhere (Cancedda et al. 2012; Ohira et al. 2014; Santucci et al. 2012; Tavella et al. 2012; Sandona et al. 2012; Camerino et al. 2013).

2.2.2.2 Mice Onboard a Biosatellite: 30 Days BION-M1 Flight Campaign

The BION satellite program for investigations of microgravity changes on various biological organisms and organ systems of higher vertebrates has a long tradition in Russian spaceflight research (Ilyin 2000). In a university cooperation between the Charité Berlin, Germany, and the Institute of Biomedical Problems (IMBP) of the Russian Academy of Sciences, Moscow, Russia (kindly supported by DLR/BMWi grants), our laboratory had the exciting possibility of participating to a 30-day BION-M1 flight campaign with young adult male mice housed separately by groups of six animals per cage in a controlled animal life support device with automated food and water supply on a biosatellite flown to orbit by a Soyuz-2 rocket (Andreev-Andrievskiy et al. 2014). The flown mice that returned back to Earth in life and in good health were sacrificed 24 h after landing by a dissection team at IMBP, and various tissues were distributed to each laboratory according to a special tissue preservation plan (sample preparation) and according to a dissection schedule consented by all investigators prior to end of the 2013 BION M1 mission (Fig. 2.12). Our laboratory received samples from six different skeletal muscles



Fig. 2.12 The BION-M1 biosatellite flight experiment scenario (April 19 to May 19, 2013). The BION M1 biosatellite with mice and other biological samples was flown by SOYUZ-2 rocket to near orbit (575 km altitude, x477 orbital circulations) and returned to Earth (Kasachstan, Russia) after 30 days (*upper left*) with soft landing system. Flown mice were harvested on landing site and delivered to the IBMP, Moscow, 11 h post landing (*upper right*). Three C57Bl/6 SPF mice (aged 4–5 months, approx. 28 g b.wt. each) were housed in a small container (lower left showing 4 of 5 module containers) with food and water ad libitum, 12 h light/dark cycle, and under ambient environmental parameters (21 °C temperature, 60 % rel. humidity, pO₂ 140–180 mmHg concentration, pCO₂ traces). Mice were sacrificed, and tissue samples prepared by a well-experienced team of scientists (*lower right*), frozen fixed, and delivered to the principal investigator's laboratories (Images: IMBP, Moscow, Russian Federation)

from five spaceflown mice each ($n = 5$, BION flight) and from a number of age- and sex-matched mice from three control groups (BION ground, flight control, vivarium control, each $n = 6$ or $n = 8$) that are currently being analyzed.

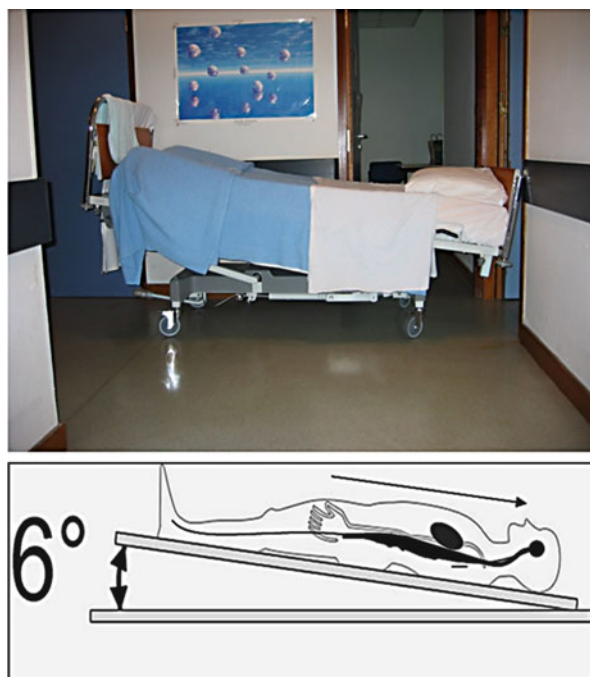
Preliminary results obtained from first analysis of the BION samples confirmed that the postural soleus and the longissimus dorsi back muscle of flown mice are highly atrophic compared to ground-based controls (ms. in preparation). In addition, intensity of the NOS1 immunoreactivity is changed in the soleus muscle compared to ground controls confirming the presence of microgravity-induced control mechanisms related to the muscular NOS/NO system in mice previously found in HU-unloaded rats (Sun et al. 2013) but also in disuse atrophy in bed rest (Rudnick et al. 2004). Further analysis, for example, on the transcriptional level, gene expression, and various putative muscular signaling pathways involved in gravitational unloading mechanisms, is currently under way.

2.2.3 Human Studies (Bed Rest)

In bed rest studies, the human body is positioned recumbent in special clinic beds usually with six-degree head-down tilt, HDT (Fig. 2.13), to study the effects of immobilization on the unloaded healthy human body during or after short-term- (>7 days), medium-term- (>21 days), and long-term-duration (>60, 90, or 120 days) bed rest in controlled laboratory environments such as provided by transitional bed rest wards (infirmary rooms) provided by university hospitals (Charité Berlin) and more specialized bed rest facilities such as provided by the National Aerospace Institute, Cologne (DLR, :envihab, Germany), and the Medical Space Clinics (MEDES) in Toulouse, France, in Europe. The HDT supine position results in partly unloading of the body with a concomitant body fluid shifting from lower to upper body parts (centralization of venous blood). An increased preload (venous return flow to the right atrium of the heart) in the cardiovascular system results in endocrine stimulation (atrial natriuretic protein secreted from heart atrium) with an enhanced renal fluid and mineral (Na^{2+} , Ca^{2+}) excretion that is even more intensified by bone mineral turnover and loss during the bed rest period (LeBlanc et al. 2007).

Immobilization-induced human body unloading results in reduced muscle tone and neuromuscular activity (hypokinesia) of trunk, back, and leg postural (anti-gravity) muscles which also result in typical structural changes (e.g., muscle volume and myofiber size reduction, myofiber slow-to-fast-type transition, altered

Fig. 2.13 A typical 6° head-down tilt (HDT) bed rest scenario/spaceflight analogue. *Upper panel* shows an empty bed at HDT position at the corridor of MEDES Space Clinics, Toulouse, France. *Lower panel* shows that volunteers at HDT supine body position are challenged by cephalad fluid shift (toward head) and partial unloading with disuse atrophy particularly of leg skeletal muscles throughout the entire bed rest period of weeks or months (spaceflight analogue model) (Images: D. Blottner)



capillary-to-myofiber ratios, intermuscular adipose tissue) and functional changes (e.g., fatigue resistance, loss in power and force, reduced neuromuscular activity) observed after extended muscle disuse (Clark 2009). As a consequence, body immobilization with hypokinesia in HDT results in disuse-induced loss of bone and muscle mass (estimated atrophy rate 1–3 % per week HDT) with reduced muscle strength (power and force) and, finally, also impaired performance control similar to the known challenges observed in crew members in microgravity in Space or after return to Earth. Since decades, HDT bed rest has been considered as an experimental analogue to spaceflight on the ground that is controlled more easily and with statistically sufficient high numbers of voluntary subjects at more economical costs and with less health risks than for human experiments with crew members under real microgravity environments (Convertino et al. 1989; LeBlanc et al. 1997). At end of a bed rest study, the volunteers are slowly accustomed to an upright body position with the help of a tilt table (orthostatic stimulation) and become instantly part of a post-recovery and rehabilitation protocol that usually is completed after 6 months or 1 year following bed rest and that again may allow for recovery studies after reloading of the human body comparable to gravitational reloading studies in spaceflown crew members after their return to Earth. Even though musculoskeletal and neuromuscular changes found in HDT are largely the same found in spaceflight or after return thereafter, it is quite reasonable that a number of other microgravity challenges for the deconditioned human body in real space missions (e.g., radiation, stress, proprioception, autonomic dysregulation, immunosuppression, vestibular control) or, for example, extreme physical and/or cognitive inflight challenges of crew members (mission duties, extravehicular activities) may not be adequately simulated by the bed rest paradigm with “terrestrial astronauts” at 1 G, for example, simulating μ G-induced changes in postural reflexes, sensorimotor behavior, and visual-vestibular neural stimulation (Reschke et al 2009). As animal study results may not be transferred 1:1 to human physiology, the use of countermeasures of various modes (e.g., exercise, nutrition) can be tested only in bed rest for their feasibility and effects on disuse-induced muscle and bone loss on Earth with the possibility for their implementation to future inflight countermeasure protocols during long-term space missions to the Moon or Mars (Pavy-Le Traon et al. 2006).

2.2.3.1 Methods I: Muscle Biopsy

Many of the structural changes and in particular the muscle-specific cell signaling adaptation in disused human skeletal muscle cannot be studied in body fluids (saliva, blood, urine) from subjects. In contrast to functional bone markers detectable in body fluids, reliable serological muscle loss markers are presently not available (Nedergaard et al. 2013). Therefore, in order to study structural adaptations including muscle-specific signaling in disuse, a small amount of muscle tissue (biopsy) needs to be taken from a well-palpable skeletal muscle at a well-known anatomic site with minimal risks of neurovascular injury (blood vessels and nerves)

and with minimal to moderate risks for discomforts (e.g., pinching pain, local hematoma, infection, scar formation). A muscle biopsy can be harvested by an experienced operator from well-palpable leg muscles of voluntary human subjects or crew members using the well-established needle biopsy technique (Bergstrom 1975). The so-called Bergström needle consists of a small hollow needle (12–15 gauge size) that is used to percutaneously harvest a small muscle tissue sample after local skin cleaning and anesthesia without or with suction modification (Tarnopolsky et al. 2011). The local anesthesia using lidocaine with epinephrine (usually injected to skin, subcutis, and fascia to help control incision-related bleeding) may, however, confound molecular analysis in needle biopsies that should be avoided by a more careful injection approach (Trappe et al. 2013). The Duchenne-Bergström percutaneous needle biopsy technique routinely gains a rice corn-sized tissue sample of about 100 mg > 150 mg of tissue (single pinch) routinely used in many previous human physiology studies, in bed rest, but also in crew members (Fig. 2.14). Currently, thinner needles are available recovering about 4 mg of tissue (single recovery) from the human vastus lateralis or from the latissimus dorsi back muscle that may open up new anatomical sites and functional muscle types to be analyzed, for example, by molecular tools where a few mg of sample amount is sufficient enough for molecular analysis (Paoli et al. 2010). Alternatively, a Rongeur surgical forceps developed to cut away bone and tough tissues has been used for a biopsy of soft muscle tissue (<150 mg) through an approx. 1 cm skin/fascia incision following local anesthesia in bed rest studies (Rittweger J, personal communication). In all cases, routine medical wound care (medical plaster) and, if necessary, anti-scar bandage with pressure dressing are applied to the small skin wound on the day of biopsy. The quality of the small tissue sample (fiber orientation, fascia and connective tissue impurities, blood coagulate)



Fig. 2.14 Typical scenarios of human skeletal muscle biopsy tissue sampling (*right*, needle biopsy) and sample collection (*left*) using color-coded microcups for muscle team principal investigators (PIs). Image (*left*) taken from the 90 days LTBR study at MEDES, Toulouse, France, and (*right*) from the 60 days BBR-2 study at the Charité, Campus Benjamin Franklin, Berlin, Germany, 2007. In the BBR-2 study, an open incision biopsy procedure was used (Belavý et al. 2010) (Images: D. Blottner)

is instantly inspected under a binocular microscope, while the sample is cleaned of non-muscle tissue, cut to smaller aliquots as required (e.g., according to histology, biochemical and molecular tissue preparations), immediately frozen in liquid nitrogen (or treated for other preservation methods required), and usually stored at minus 80 °C freezer (or in 4 °C refrigerator) for further sample analysis in a laboratory on site or at home.

Due to sharp edges and scoop-shaped tips, both Bergström needle and Rongeur forceps share some risks of partial mechanical stress to the soft muscle sample that may interfere with a more broad tissue analysis including routine histology, ultra-structural analysis, and routine biochemical or sophisticated proteomic analysis. Some difficulties in biochemical and molecular measures caused by the needle biopsy protocol were reported that may result in variable changes in immunoblot signals, for example, when muscle samples were to be analyzed for cell signaling in human tissue (Caron et al. 2011). In order to minimize any mechanical stress during biopsy sampling and to improve tissue quality and quantity, an open incision biopsy technique has been alternatively used in two ESA long-term bed rest studies at the Charité Berlin (2003 Berlin Bed Rest (BBR)-1 and 2006–2007 BBR-2 study) that resulted in the sampling of muscle tissue of excellent quality (longitudinal fiber orientation) and quantity (>250 mg/biopsy) from the thigh (quadriceps femoris vastus lateralis) and the deep calf muscle (soleus). After local skin/fascia anesthesia, an approximately 1.5 cm skin/fascia incision is made, and a small bundle of muscle fibers is ligated and carefully separated from the adjacent fiber bundles of the muscle under visual control. Following proximal and distal cutting, the small ligated fiber bundle (approx. 300–400 fibers in longitudinal orientation) is then directly excised from the periphery of muscle by a surgeon, immediately handed over to another operator for further sample preparation, freezing, and storage. Meanwhile, both fascia and skin are sutured in situ (2–3 sutures) followed by normal wound care as shown in the BBR-2 study protocol paper (Belavý et al. 2010).

The open incision biopsy is a safe alternative to the standard needle biopsy but requires a well-trained surgeon and a surgery room of a clinic in a hospital. As already outlined, the latter technique has some advantages over the needle biopsy by getting “gold standard” biopsy samples from human skeletal muscle with much less mechanical manipulations and better histologic tissue preservation. High-quality biopsy material of sufficient amount is therefore proposed for comprehensive multidisciplinary human studies in future Space Life Sciences where ultrastructural/histological/high-resolution confocal laser structural analysis needs to be combined with molecular cell biology and sophisticated -omics technology (prote-/transcript-/metabol-/signal-omics) to get more comprehensive insights by using interdisciplinary tissue analysis to further understand the normal and abnormal mechanistic control and maintenance levels of disused skeletal muscle (Moriggi et al. 2010; Salanova et al. 2014) as a valuable on ground data base for comparison with the microgravity-induced changes in skeletal muscle atrophy.

The human skeletal muscle system is comprised of different muscle types with different functions (postural control/stabilization vs. fast mobilization) and

different myofiber distribution patterns (type I, IIa, IIx) typical to a given muscle that appear to also respond in a typically muscle-specific way to disuse and exercise. Due to different physical training, routine daily activity patterns, endocrine status (sex hormones), and age, human skeletal muscle may show a high intersubject variability that should be considered for the study design in Human Space Life Sciences, for example, with study inclusion of sex- and age-matched subjects. For standardization, a biopsy is usually taken from at least two muscle types with a different fiber-type composition, e.g., the mixed fast/slow fiber composition thigh muscle (vastus lateralis) and the more slow fiber composition calf muscle (soleus), as reference muscles due to the fact that a wealth of structural and functional data was accumulated from these muscle types in many human studies on the ground and from spaceflight experiments over the last two or three decades.

In bed rest, a muscle biopsy is usually taken from volunteer subjects (male or female) after signed informed consent briefing before start of bed rest (pre-biopsy) and at the end or after bed rest (post-biopsy) in order to investigate short-, medium-, and long-term skeletal muscle changes and their possible prevention by countermeasures at various structural and molecular levels, for example, in bed rest subjects or crew members. If exercise interventions were applied as countermeasures in disuse on the ground or during the crew member's preflight training, the test constraints include no strenuous exercise during 24 h prior to the biopsy, no exercise on the biopsy day, or working out of the biopsied muscle/leg for at least 24 h after the biopsy. In human spaceflight experiments, usually a preflight (several weeks before launch) and one or two postflight biopsies (shortly after landing/after 1–2 weeks of recovery) might be taken from the crew members (presently using standard needle biopsy).

Inflight muscle biopsies may not be feasible in the near future in fact due to ethical and safety reasons because wound healing and the associated pathophysiological processes under microgravity conditions are not yet fully understood (Davidson et al. 1999), and thus more serious risks (inflight emergency) may not be excluded for the crew during their mission duties in Space.

2.2.3.2 Methods II: High-Resolution Confocal Laser Scanning (CLS) Microscopy

Skeletal muscle atrophy is paralleled by histological changes in myofiber size (myofiber cross-sectional area) and myofiber phenotype distribution (slow type 1, fast type 2a, 2x) that have been investigated in biopsy tissue sections (paraffin or cryosections) by standard histochemistry and immunohistochemistry methods with conventional light and fluorescence microscopy. With the development of more stable (less bleaching/fading) fluorescence signal-conjugated secondary antibodies (e.g., Alexa 400, 488, 550, 630 nm, molecular probes) in combination with double and triple immunostaining protocols in one and the same muscle cryosection, high-resolution three-channel confocal laser scanning (CLS) microscopy became the method of choice for specific antibody detection following

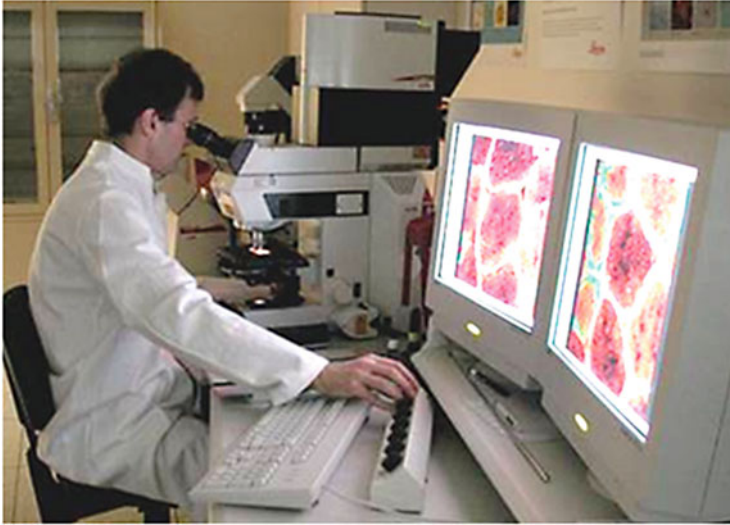


Fig. 2.15 Confocal laser scanning (CLS) microscopy device (Leica TCS SP-2, leica-microsystems.com) used in the Neuromuscular Group laboratory at the Charité Universitätsmedizin Berlin, Germany, since 2001 (DLR grant # 50WB0145 to D.B.)

multiple immunostaining protocols for high resolution of particular functional muscle cell structural and functional biomarkers relevant for various subcellular compartments (e.g., sarcolemma, sarcosol, contractile apparatus, neuromuscular junction) as well as for muscle-specific signaling pathways (Fig. 2.15). Briefly, confocal laser image analysis is achieved by the stepwise optical dissection planes through 8–30 micron (μm) thick cryosections (comparable to a high-resolution cell CT using a stable laser light source instead of X-ray). The optical dissection steps by the highly sensitive laser beam-splitter technology can be preset to variable consecutive optical planes (e.g., $0.01 \mu\text{m}/\text{step}$), thus leading to a precise signal detection of various fluorescent biomarkers (red-green-blue) at subcellular compartments (without diffuse and nonspecific signal noise often detected with immunohistological sections by routine epifluorescence microscopy).

2.2.3.3 Muscle and Fiber Size (CSA) and Fiber-Type Distribution (Slow/Fast) in Bed Rest

The loss in muscle mass during immobilization also termed disuse atrophy (muscle wasting) has been determined in bed rest noninvasively mainly in human postural muscles by routine clinical imaging techniques. For example, the disuse-induced structural size of whole skeletal muscle cross-sectional area (MCSA) was routinely monitored by magnetic resonance imaging (MRI) that, for instance, gives reproducible muscle volume image data sets from individual deep back muscles (e.g., multifidus) and the calf soleus known for their strong atrophy responses following

longer periods of disuse (Belavý et al. 2011). In addition, whole body MRI screening in bed rest revealed that the magnitude of MCSA reduction in postural but also in other limb and trunk muscles may be region-specific and not uniform within a given muscle but may rather show variable sites of atrophy throughout the full length of a muscle (Miokovic et al 2012). Alternatively, high-resolution ultrasound (ultrasonography, echography) that may be more easily applied in bed rest has been used more recently to noninvasively monitor MCSA in normal subjects (Esformes et al. 2002), following high-intensity muscle training (Ahtiainen et al. 2010), and in bed rest (Arbeille et al. 2009) with reproducible and valid results and comparable degree of precision to MRI.

Nevertheless, in vivo anatomical variability may be found in axial cross sections, for example, at mid-thigh or calf bone, muscle, and related neurovascular structures (regional nerves and blood vessels) at the human limbs often showing region-specific interfascial tissue spaces or variable intermuscular and intramyocellular fat infiltrations or deposits. It is also known that acute or strenuous exercise in normal subjects usually results in post-training edema that may last for up to several hours following exercise intervention, for example, reported for the human thigh muscle (Ploutz-Snyder et al. 1997) which may also likely occur in long-term bed rest following strenuous exercise interventions as countermeasures. In addition, significant differences in size measurements were reported between recumbent versus standing MRI measures (Berg et al. 1993), and the known cephalad (head-directed) fluid shift from the legs to the upper body during supine bed rest (Thornton et al. 1992) may still provide a yet underestimated bias in the morphometric analysis of whole skeletal muscle size, for example, by X-ray-based technology (Rittweger et al. 2013). Unlike for bones, tendons, or even strong fascia layers, the current available routine and more advanced digital imaging technology for soft tissues based on gray-scale determination (MRI, ultrasound, spectroscopy, X-ray based) still does not provide adequate signal-to-noise resolution criteria for the clear signal discrimination between the various body soft tissue compositions and their individual components such as water, fat, blood, or lymph fluid versus connective and soft tissue that may at least partly add to the variable size changes particularly found in disused human limb tissue including skeletal muscle and support tissue structures in long-term bed rest. Yet limited evidence for reliability of the current MRI measures or even of real-time ultrasound measures in routine human limb muscles size monitoring in clinical settings (English et al. 2012) as well as in bed rest immobilization is still critical. There is a need for advanced technology with, for example, a better signal resolution and discrimination between more discrete signals of various biological tissue components to properly study atrophy and size changes in addition to noninvasive monitoring of muscle volume changes that are required in future bed rest studies. Though the presently available MRI techniques used in routine clinical imaging may be helpful for diagnostic purposes, they may only show larger volume changes of the whole muscle tissue (and its non-muscle components and fluid content) under prolonged bed rest conditions without excluding the obvious bias of over-/underestimations of the actual magnitude of structural myofiber atrophy actually found in the various fibers

of intramuscular fascicles and, more importantly, detectable by variable size changes of individual myofiber phenotypes (slow, fast), for example, only by high-resolution confocal laser scanning microscopy.

2.2.3.4 NO/NOS as Biomarker to Study Efficacy of Physical Exercise Countermeasure

Emerging evidence accumulated showing that biological NO signals have multiple functions in normal skeletal muscle including muscle contractility, soreness, and fatigue that altogether are typically known as skeletal muscle functional impairments following various periods of disuse on the ground or that have been reported from crew members during spaceflight missions and following recovery thereafter (see Sect. 2.1.6.). We therefore hypothesized that NO signaling may be altered in normal human skeletal muscle following disuse and that changes in NOS/NO can be ameliorated if not prevented by physical exercise as countermeasure during the periods of disuse in bed rest. In particular, we were interested to know if NOS/NO could be used as a reproducible and reliable structural and functional biomarker for muscle activity versus inactivity for testing of the efficacy of an exercise countermeasure protocol during bed rest disuse.

One of the first evidence of atrophy-induced changes in NOS1 in normal human skeletal muscle was reported from our immunohistochemical analysis of all three NOS isoforms (NOS1, NOS 2, NOS3) in muscle biopsy material originating from a 90-day ESA long-term bed rest study performed in 2001 at the MEDES Space Clinics in Toulouse, France (Rudnick et al. 2004). In this study, we showed substantial loss in NOS proteins in human muscle biopsy lysate preparations from slow- and fast-type muscle (VL, SOL) of the bed rest control group (bed rest, no exercise) compared to normal control (before bed rest). By contrast, maximal force resistive exercise countermeasure performed in a bed rest resistive exercise (RE) group (fly wheel technology, 3×20 min/weekly) prevented such changes almost completely in both VL and SOL suggesting that the quantity of muscular NOS is activity driven and that in principle exercise is able to maintain the NOS1 myofiber status in human skeletal muscle in longer periods of disuse (Fig. 2.16).

We also found in this study that NOS2 (inducible NOS) is co-localized to caveolin-3 (important signal component of the muscle membrane) at the human sarcolemma and is highly regulated by resistive exercise and NOS3 (endothelial NOS) is upregulated by resistive exercise in the microvascular/capillary bed surrounding the muscle fibers in the trained bed rest group (Rudnick et al. 2004). These results were largely confirmed by the second ESA Berlin Bed Rest Study in 2003, BBR-2 (Blottner et al. 2006), and also following 7 and 14 days' human unloading study of "dry immersion" (Koryak 2002) without or with plantar support stimulation in a cooperation experiment between the Charité Berlin and the IMBP, Moscow (Moukhina et al. 2004). Briefly, plantar stimulation appears to be a very effective way of dynamic biomechanical stimulation applied to the skin mechanosensors (PACINI bodies) of the foot sole of the unloaded human leg that positively affects

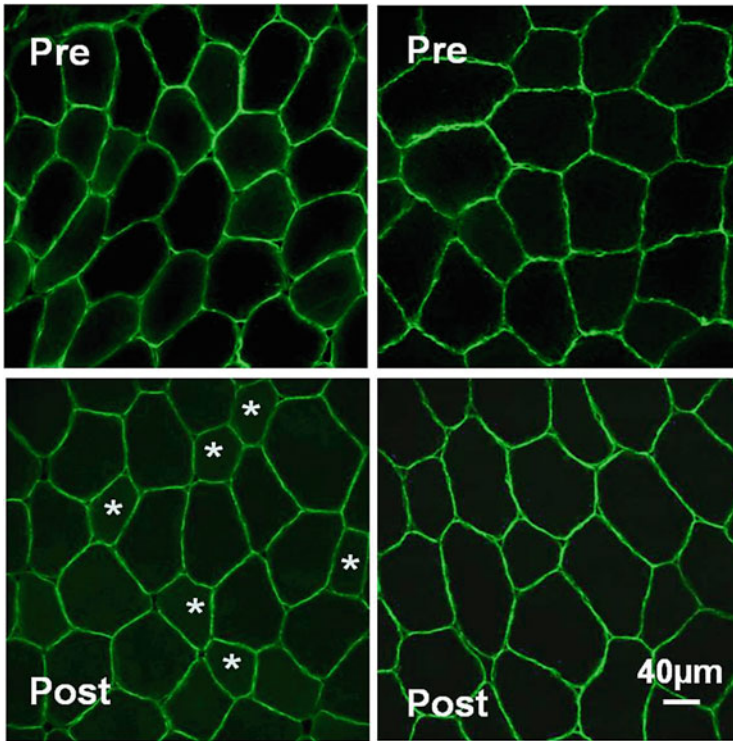


Fig. 2.16 Sarcolemmal NOS1 immunostaining in human skeletal muscle fibers before (Pre) and after bed rest (Post) without (*left column*) and with exercise (RVE) countermeasure (*right column*). The intensity of sarcolemmal NOS1 immunosignals is maintained after exercise (Rudnick et al. 2004). Asterisks denote atrophic myofibers with diffuse cytosolic NOS1 immunostaining (60-d BBR-1 study, Charité Berlin, Germany)

the calf muscle tone and contractile properties while the body is floating “dry” in a water tub (dry immersion) separated by a thin water-resistant membrane established and performed at the Institute of Biomedical Problems (IMBP) of the Russian Academy of Sciences in Moscow, Russia (Koryak 2002).

In animal studies, muscle-specific splice variant μ NOS delocalization inhibits muscle force in dystrophin-null mice suggesting nitrosative stress elicited by NO generated by NOS as inhibitor in muscle force generation (Li et al. 2011). Knockout (KO) experiments (μ NOS^{-/-}) in mice resulted in myopathy and reduction in contractile force, thus underlining the key role of NOS in muscle force production (Percival et al. 2010). Two animal studies furthermore suggested involvement of endogenous NO production inhibited by L-NAME (potent inhibitor of NOS) in chronic overload-induced skeletal muscle hypertrophy of rat plantaris muscle and myofiber-type transition (Smith et al. 2002) or in activity-induced calcineurin-NFATc1 signaling (involved in activity-dependent myosin heavy chain isoform expression) and fast-to-slow skeletal fiber-type conversions (Martins et al. 2012).

In normal human skeletal muscle, we also observed an altered expression of sarcolemmal NOS following longer periods of disuse and exercise. After long-term bed rest (LTBR 2001), for example, we found that the loss of sarcolemmal NOS localization in atrophied human soleus myofibers can be prevented by maximally resistive exercise as countermeasure (fly wheel technology) compared to a non-exercising bed rest control group suggesting that sarcolemmal NOS is activity dependently expressed in human skeletal muscle (Rudnick et al. 2004). In a 60-day bed rest study (1st Berlin Bed Rest Study, BBR-1, 2003, Blottner et al. 2006), we showed that the sarcolemmal NOS expression can be maintained by whole body resistive vibration (RVE) which represents a short but high-intensity stimulation training protocol applied to subjects during bed rest (approx 10.000 muscle contraction cycles 2–3x/week for 3–5 min) compared to the relatively exhaustive RE fly wheel technology (performed for 20 min for 3 days/week). Thus, vibration may be a highly effective biomechanical signal for human muscle that may be useful to maintain functional NOS following longer periods of immobilization such as in bed rest or during real spaceflight. In a follow-up 60-day bed rest study (2nd Berlin Bed Rest, 2006), we compared the training effects in bed rest between two different resistive exercise RE groups, RE only (RE without vibration) and RVE (RE plus vibration), on various structural skeletal muscle parameters. Notably, both RE and RVE protocols performed on the same Galileo Space® trainer (MediTec, Pforzheim, Germany) maintained sarcolemmal NOS localization patterns supporting the general idea of the presence of an activity-driven NOS expression. If similar findings were obtained from crew members in real spaceflight, it will be investigated in future planned work.

Disruption of the subsarcolemmal localization of NOS1 (nNOS) appears to be a signature of fiber atrophy in animal and human normal skeletal muscle fibers with as yet unknown consequences (Miyagoe-Suzuki and Takeda 2001). A more recent report on the NOS sarcolemma-sarcosolic translocation mechanisms suggested that the cell permeable, saline-manganese compound EUK-134 (Lawler et al. 2014) ameliorates NOS translocation in 54 h hind-limb suspended adult F344 rats which also suggest involvement of redox signaling that may be either decreased or increased following muscle unloading (2.2.3.5, nitrosative stress). From fundamental animal studies on ground as well as in microgravity, we suggest that the quantity changes of sarcolemmal NOS expression at the outer muscle fiber membrane likely reflected some fundamental mechanistic principles and their changes in the molecular microdomain membrane composition in skeletal muscle disuse that need to be further investigated. A more recent work shows that the stress protein/chaperone GRP94 which binds to NOS mechanistically stabilizes the NOS multiprotein complex at the myofiber sarcolemma (Vitadello et al. 2014). The changes in sarcolemmal NOS expression have been also reported in various human skeletal muscle dystrophies (e.g., Chao et al. 1996; Crosbie et al. 2002; Tidball and Wehling-Henriks 2004; Fanin et al. 2009), suggesting aberrant sarcolemmal NOS localization patterns as valuable pathophysiological markers in various myopathies that may be helpful in their clinical diagnosis (Zhou and Zhu 2009).

In spaceflown mice skeletal muscle (see Sects. 2.2.2.1 and 2.2.2.2), we found that translocation of sarcolemmal NOS to sarcosol is particularly apparent in

atrophic soleus but not in the extensor digitorum longus (EDL) compared to ground controls (Sandona et al. 2010) supporting coexisting mechanisms of disuse atrophy and NOS translocation are signatures to microgravity disuse atrophy.

2.2.3.5 Skeletal Muscle Say “NO” to Disuse on Earth: NO and Nitrosative Stress in Human Skeletal Muscle

Nitric oxide synthase (NOS) and the diffusible NO signals are expressed in animal and human skeletal muscle with pleiotropic biological roles for normal skeletal muscle structure and function (Bredt and Snyder 1994; Kobzik et al. 1994). Depending on muscle activity or inactivity, muscular NOS proteins and NO signals are either up- or downregulated; NOS1 is translocated in myofibers from sarcolemma to the sarcosol in animal and human muscle disuse and myopathies, as well as in spaceflown mice (see Sects. 2.2.2.1 and 2.2.2.2). Uncontrolled over-/underproduction and/or aberrant expression of free radicals (Lawler et al. 2003) such as superoxide (O_2^-) or nitric oxide (NO) in skeletal muscle tissue provide the basis for oxidative/nitrosative stress that is induced by reactive oxygen/nitrogen species (ROS/RNS).

Nitrosylation of proteins is characterized by the covalently binding of NO to reactive free cysteine residues ($-SH$ groups) of a protein that are instantly converted to S-NO groups recently identified and listed by functional target SNO-proteins of the SNO-proteome (Seth and Stamler 2011). In analogy to phosphorylation and acetylation of functional cell peptides/proteins, the term nitrosation or S-nitrosylation has been proposed for SNO-protein modifications (Fig. 2.17) which are supposed to

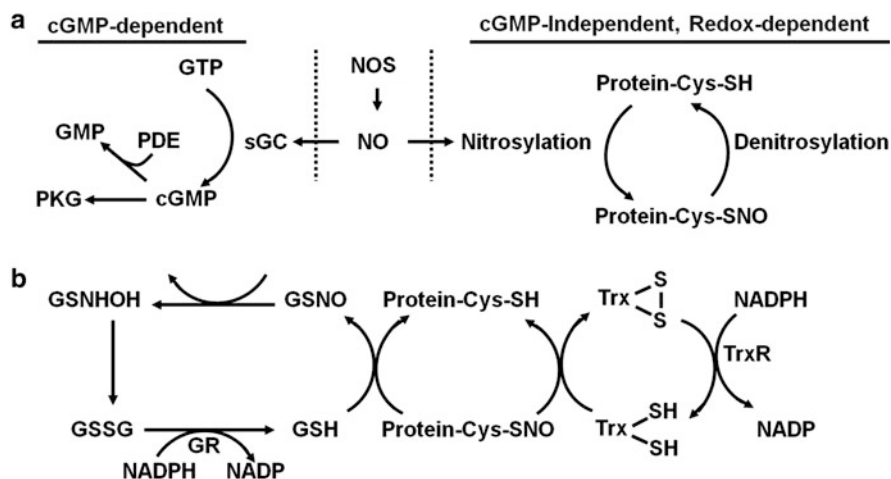


Fig. 2.17 Scheme showing protein-S-nitrosylation (SNO-proteins) via NO-based signaling. Nitrosylation of proteins (protein-Cys-SNO) is a cGMP-independent but redox-dependent mechanism that is (a) driven directly by NO (*upper middle panel*) and (b) by glutathione (GSH, *left panel*) and thioredoxin reductase (TrxR, *right panel*), for reversible protein nitrosylation/denitrosylation (*lower middle panel*) via NADP-dependent redox mechanisms (Lima et al. 2010)

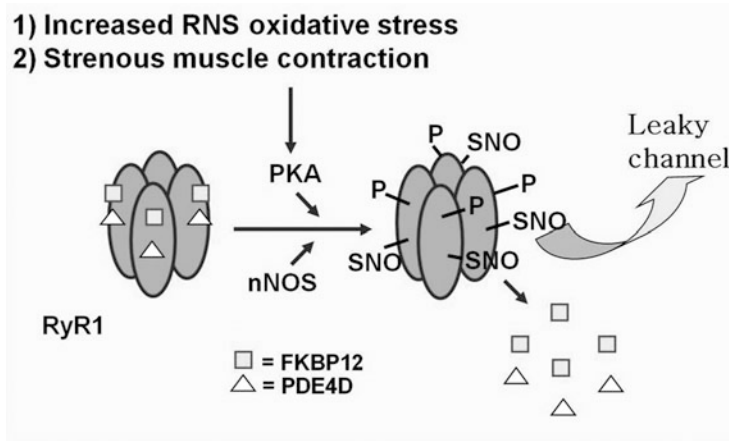


Fig. 2.18 Proposed model of nitrosative stress by reactive nitrogen species (RNS) for decreased exercise capacity. Ryanodine receptor proteins (RyR1) are hyper-nitrosylated (SNO) via nNOS and hyperphosphorylated via protein kinase A (PKA) resulting in leaky channels with myocellular calcium imbalance

have a tissue half-life of approximately a few seconds to a few minutes maximum in biological tissues (Foster et al. 2009). Under normal physiological conditions, S-nitrosylation is a reversible posttranslational qualitative modification of functional proteins and a major source of NO bioactivity, thus regulating cell dynamics and plasticity in a variety of tissues and cells (Hess and Stamler 2011). In many cell types and tissues including skeletal muscle, also the quantitative nitrosylation via unbalanced NO cell signals (hyper-/hyponitrosylation) either stimulates, maintains, or even suppresses control mechanisms of functional cell proteins (Eu et al. 2003) such as those shown for the myosins of the contractile apparatus (Nogueira et al. 2009), for the sarcoplasmic reticulum (SR) calcium release channel protein ryanodine receptor type-1 (Fig. 2.18, Bellinger et al. 2008; Salanova et al. 2008), and for a number of other calcium release channels (Aracena et al. 2005). For example, calcium release channel proteins such as RyR1 may become “leaky” in the presence of too much of NO which may result in muscle stiffness and lack of force production (Powers et al. 2007). Muscle disuse atrophy also induces oxidative stress that accelerates protein degradation via increased substrate recognition of oxidized proteins by the E3 ligases (MuRF1-3) that, in turn, promote their susceptibility to proteolysis (Powers and Lennon 1999; Du et al. 2004).

We were able to show that activity-induced NO imbalance and nitrosative stress are proposed mechanisms of disrupted calcium homeostasis in disuse atrophy of normal human skeletal muscle in bed rest (Salanova et al. 2013). In muscle biopsies obtained from the 60-day BBR-2 study at the Charité Berlin, Germany (2007–2008), we investigated differential levels and expression of functional SNO muscle proteins of the excitation-contraction (EC)-coupling machinery related to the control of calcium balance in muscle, for example, ryanodine receptor type 1 (Salanova

et al. 2008, 2009), but also voltage-dependent calcium release (DHPR1a) and calcium uptake proteins (SERCA1&2, PMCA1) in chronically disused normal skeletal muscle in bed rest using a modified biochemical assay for the detection of SNO-proteins in cell and tissue samples (biotin-switch technique, Jaffrey and Snyder 2001) in combination with high-resolution confocal image analysis and real-time quantitative polymerase chain-reactivity (qPCR) analysis of Nrf-2 transcripts, a master gene which activates the transcriptional activity of antioxidant responsive elements (AREs) of many cytoprotective genes in the cell nuclei, in soleus, and in vastus lateralis muscle fibers in bed rest following two types of resistive exercise, RE and RVE, as countermeasure (Salanova et al. 2013). Compared to control baseline levels (bed rest start) and to the non-trained bed rest control group (bed rest end), most of the functional SNO-proteins investigated in the exercise group (RyR1, SERCA, PMCA, myosins) were downregulated, while others were maintained following either of the exercise protocol after chronic disuse in bed rest. Interestingly, variably nitrosylated NOS1 (SNO-NOS1) protein levels were found after chronic disuse in bed rest (SNO-NOS1 decreased) and following exercise countermeasure during bed rest (SNO-NOS1 increased) suggesting also NOS1 being a novel candidate in the growing list of muscular SNO-proteins (Fig. 2.19) that share activity-driven autonitrosylation mechanisms to occur with as yet unknown functional significance for the physiological and molecular control of a NOS1 activity and myocellular NO production in a muscle-specific way (Salanova et al. 2013).

Like other SNO-proteins, we propose that NOS1 may be controlled in skeletal muscle fibers, for example, by S-nitrosylases and denitrosylases (Jaffrey et al. 2001; Seth and Stamler 2011). Previous animal studies reported protein nitrosylation to be

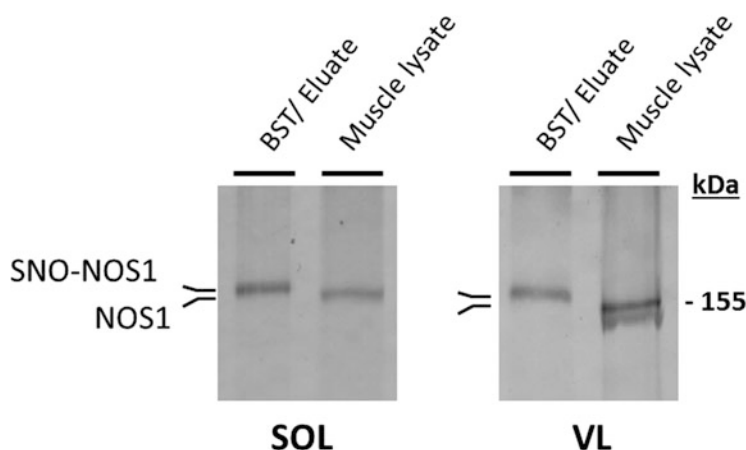


Fig. 2.19 The NOS1 protein itself is S-nitrosylated as shown by molecular weight shift of SNO-NOS1 seen in human soleus (SOL) and vastus lateralis (VL) protein BST/eluates compared to controls (muscle lysate) identified by a modified biochemical BST-based protein-S-nitrosylation assay (Salanova et al. 2013)

responsible for increased *in vivo* proteolysis in cirrhotic rats (Wang et al. 2010). Nevertheless, aberrant levels of functional SNO-proteins are a signature of differential nitrosative stress management in atrophic/disused versus trained human skeletal muscle related to calcium balance (Salanova et al. 2013).

As already shown for reactive oxygen species in exercise biology (Ji 2008), a contraction-induced overproduction of reactive nitrosative species and nitrosative stress in muscle likely occurs following maximally heavy loading bouts under extreme training conditions (overload) or by extremely long-duration exercise (marathon runners) in sports which might explain some of the changes observed in remarkably small subsets of muscle genes (P13K/Akt/mTOR, Foxo transcription factor, atrogin-1, MuRF1/Mafbx, myostatin) that, when turned on (activated) by unloading/disuse, may trigger discrete molecular pathways that lead to atrophy in various atrophy models (Urso et al. 2009) or that, when turned off (suppressed) by normal muscle activity and by exercise, may trigger molecular signaling mechanisms of structural muscle fiber preservation, such as size and phenotype distribution, and functional muscle fiber parameters, such as contractility, reduce fatigue, and/or maintain force production in normal and exercise physiology (Suhr et al. 2013). A current report addressing the NOS/NO signaling pathway mechanisms suggested that the NOS1-activated NADPH oxidase NOX4 may contribute to fiber hypertrophy in the overloaded skeletal muscle (Ito et al. 2013). Likewise, uncontrolled excess of reactive nitrogen species and nitrosylated functional proteins (SNO-proteins) including auto-nitrosylated NOS1 (nNOS), as, for example, reported from our laboratory after bed rest immobilization may equally result in adverse nitrosative stress conditions, thus triggering disuse-induced muscle atrophy mechanisms (Salanova et al. 2013). These findings well correlated with the results reported by Bellinger et al. (2009) showing that dystrophic muscle is characterized by the presence of hyper-nitrosylated RyR1 leaky channel and by Lehnart et al. (2005) who showed that specific deletion of a cAMP-dependent phosphodiesterase (PDE4D3) in a mouse model results in expression of PKA-dependent RyR2 hyper-phosphorylated leaky channels.

In fact, unbalanced nitrosative stress management (Stein 2002; Stein and Leski 2000) in inactivity periods of skeletal muscle due to unloading/disuse on Earth may likely be one of the reasons for impaired muscle functions observed in Space as, for example, reflected by muscle soreness, stiffness, and fatigue in crew members during their missions' duties in extended spaceflight (Fig. 2.20). This most important novel finding may be of some relevance in order to develop more adequate countermeasure protocols attenuating the disuse-induced nitrosative stress mechanisms that may also trigger skeletal muscle atrophy mechanisms following body immobilization in various clinical settings, in rehabilitation, and also during micro-gravity exposure in human spaceflight or thereafter (Salanova et al. 2013).

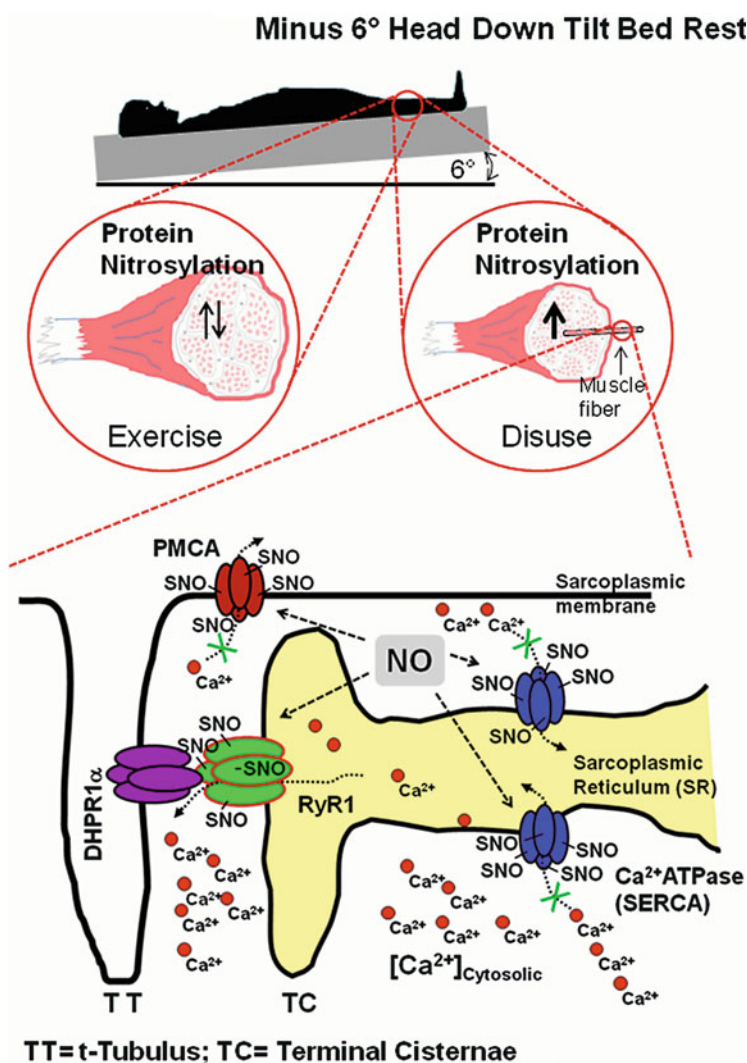


Fig. 2.20 Cartoon showing nitrosative stress management in disused human skeletal muscle studied by bed rest immobilization. Protein nitrosylation (SNO) was found to be upregulated in disused skeletal muscle and maintained at baseline following exercise countermeasure in bed rest. Lower panel shows some functional SNO-proteins (each functional receptor/channel is reflected by four subunits shown by different colors) identified in skeletal myofibers (PMCA, DHPR, RYR1, SERCA) in normal and disused human skeletal muscle (Salanova et al. 2013)

2.2.3.6 Skeletal Muscle Protein Mapping by Proteomics in Bed Rest

Proteomics is a very powerful *-omics* tool for informative mapping of the skeletal muscle protein machinery which comprises, for example, structural, contractile, metabolic, stress response, signaling, transport proteins, and probably many others.

Skeletal muscle is normally characterized by expression patterns of different structural and functional proteins (protein signature of a given muscle) that may be typical for a given muscle and that might be changed in response to adaptation processes following disuse or exercise but also in spaceflight. Proteomics is a complex laboratory-based multistep biochemical analysis including current robotic and automated technology combined with fluorescent protein dye labeling and identification using high-resolution laser scan readers and data processing using bioinformatics software (data mining via online protein banks). Two current reviews on proteomics of human skeletal muscle in health and disease are found elsewhere (Gelfi et al. 2011; Dowling et al. 2014).

Briefly, proteomics is based on a routine sodium dodecyl sulfate-polyacrylamide gel electrophoresis (SDS-PAGE) of muscle proteins extracted from individual biopsy samples in a frozen mortar by sonication in a special buffer solution (Tris/urea buffer with detergent and protease inhibitor) in two dimensions (2D). The proteins are then separated from nonprotein impurities and resuspended in lysis buffer (protein solubilization) for protein concentration determination. In the first dimension, identical amounts of proteins (40–50 μ g extract) are pre-stained with cyanine dyes such as Cy3 (red) and Cy5 (green) fluorescent label (CyDye DIGE Fluor minimal dye, GE Healthcare) and separated by isoelectric point focusing according to pH gradients with nonlinear gel strips (pH 3–10, IPG strips). In the second dimension, an SDS gel (20 \times 20 cm) is run (at 90° angle to IPG gels) to separate proteins by their molecular weights. After routine silver staining, the final 2D gels show complex protein spot patterns of different sizes and locations typical for each sample (Fig. 2.21).

In 2D-DIGE protein profiling, the CyDye-labeled proteins are furthermore identified and quantified by a fluorescent laser scanner (Typhoon 9200 Imager, GE Healthcare) using a special software package (DeCyder software, GE) and a special biological variation analysis (BVA) module for exact inter-gel spot matching and protein identification and quantification. In bed rest biopsy samples, for example, about 3000 different spots were identified from one small biopsy sample either from one muscle type or a control group muscle that can be compared to those found in a second sample from the same or another muscle type of an experimental group as, for example, required for bed rest studies (Moriggi et al. 2010). In several next consecutive steps of analysis, the area of a protein of interest is punched from the 2D gels (Ettan spot picker robotic system, GE), and the released peptides are subjected to reverse-phase chromatography (Zip-TIP C18 μ , Millipore), further processed by mass spectroscopy (MS) for protein/peptide identification, then compared with *Homo sapiens* NCBI nr Database bank (verification), and finally identified by correlation with entries in SWISS-Prot TrEMBL using ProteinLynx Global Server (Waters). In combination with MALDI-ToF/MS and HPLC ESI, the 2D-DIGE method thus provides differential maps of muscle proteins and peptides from normal versus disused muscle that give new information on the quantity and quality of protein changes (several thousands of proteins) from the proteome of a skeletal muscle of interest under normal and experimental conditions (Fig. 2.21).

In cooperation with our Italian partners of the University of Milano, Italy, proteomics (2D DIGE and MS) was used in combination with a histologic analysis

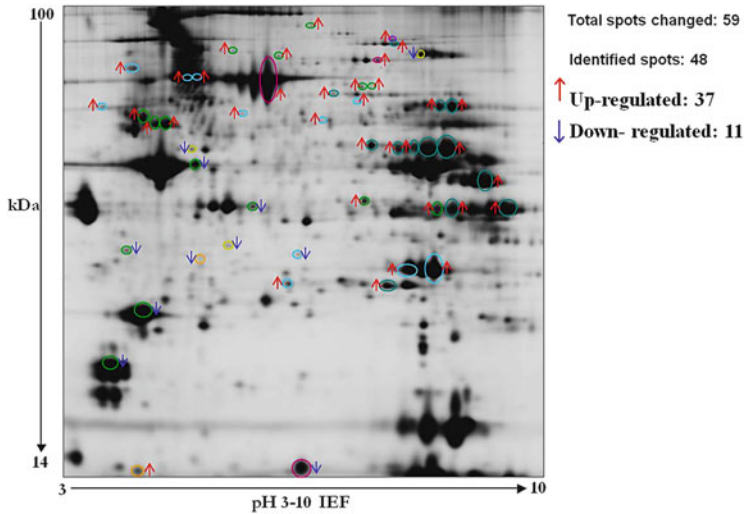


Fig. 2.21 Representative 2-DIGE protein mapping of human skeletal muscle proteome changes from soleus muscle biopsy (BBR-1 study). In the first dimension, muscle proteins were separated (first dimension) by isoelectric focusing (IEF, pH 3–10, x-axis) followed by (second dimension) molecular weight (kDa 14–100, y-axis) protein separation. From a total of 59 changed silver-stained dark spots with 48 identified spots, 37 spots were upregulated (↑, red arrows) and 11 spots were downregulated (↓, blue arrows). Individual proteins or peptides of interest are further identified by MALDI ToF/mass spectroscopy and HPLC/ESI (Courtesy: C. Gelfi (see Moriggi et al. 2010; Salanova et al. 2014))

to investigate changes in human skeletal muscle and their muscle fibers following disuse in samples from the 60-d BBR-1 study without and with vibration exercise (RVE). After bed rest, we found a substantial downregulation of proteins of the aerobic metabolism that was reversed by RVE, more in VL than in SOL. By contrast, proteins of anaerobic glycolysis were upregulated following RVE compared to bed rest without exercise countermeasure. Structural proteins from the sarcomere and the costamere microdomains were highly dysregulated by disuse and exercise (Moriggi et al. 2010).

A more detailed analysis of the structural, ultrastructural, and proteomic analysis was performed in our group with biopsy samples (SOL, VL) from the follow-up 60-d BBR-2 study (Salanova et al. 2014). In this study, we correlated some of the changes found in the proteome profiles in disused versus trained muscle in bed rest with the structural and morphometric findings from the same biopsy material following two different exercise modalities (RE vs. RVE) versus a control bed rest-only group after 8 weeks in bed rest (Salanova et al. 2014). Noteworthy, the contractile cytoskeletal and costameric proteins (tenascin-C, ROCK-1, FAK) were normalized following RVE particularly in SOL; however, costameric proteins increased by 59 % (RVE) and by 108 % (RE) versus control (no exercise). The unexpected ultrastructural damage found in bed rest after RE, but not after RVE (Fig. 2.22), was confirmed by concomitant increase in MuRF1 proteins (proteolysis biomarker) in the same

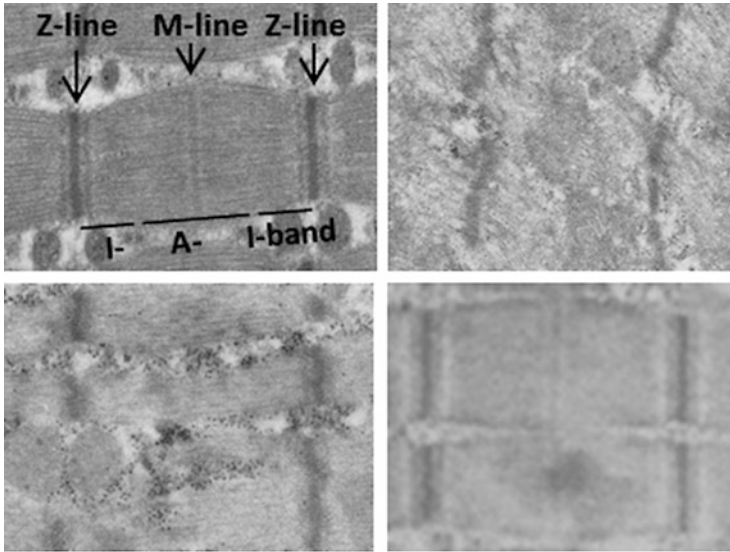


Fig. 2.22 Electron microscopy of normal sarcomeres (*upper left*) in healthy human skeletal myofibers with regular ultrastructure (regular Z-line, M-line, A-, and I-bands) and abnormal sarcomeres deteriorated after disuse atrophy in bed rest (*upper right*) showing perturbed ultrastructure. *Lower panel* shows two images of sarcomeres from soleus at identical magnifications following bed rest, with resistive exercise (RE, *lower left*) still showing signs of myofibrillar desintegration and with resistive exercise superimposed with vibration (RVE, *lower right*) with apparently regular myofibrillar orientation and normal sarcomere ultrastructure (Modified from Salanova et al. 2014)

samples. In VL, the outcome of RVE and RE on the proteomic pattern of some sarcomeric proteins (troponin, MYL2, sarcosin, desmin) was similar. As previously shown in the BBR-1 study by comparison between RVE and a bed rest control group without exercise (Blottner et al. 2006), we now provided further molecular and proteomic evidence suggesting that RE superimposed with vibration stimulation (RVE) is a highly efficient exercise countermeasure protocol against muscle atrophy, ultrastructural damage, and molecular dysregulation of basic functional muscle proteins (i.e., proteomic profiling of contractile, cytoskeletal and costameric proteins) induced by chronic disuse (Salanova et al. 2014).

In conclusion, the use of proteomics combined with structural, confocal, and biochemical analysis performed on the same biopsy material has broadened our current view on human skeletal muscle protein changes following disuse and exercise and therefore has become an inevitable and indispensable novel tool in fundamental and applied research in Human Space Life Sciences. In the near future, *omics* profiling is thought to become an indispensable new standard tool for personalized medicine in human space flight to individualize countermeasures that enhance health, safety, and performance of mission crew members (Schmidt and Goodwin 2013).

2.2.3.7 Good Vibrations Are Half the Battle Against Disuse Atrophy: Resistive Loading with Neuroreflexive Stimulation Using the Galileo® Muscle Exercise Regimen

If properly used in adequate muscle exercise protocols, vibration mechanical signals targeted to the musculoskeletal system result in exceptionally high rates of contraction cycles (approximately 1,000 cycles per second) controlled by spontaneous muscle stretch reflexes that help to mitigate disuse atrophy and reduction of neuromuscular activity in bed rest (Rittweger et al. 2010). One of the advantages of this exercise modality already addressed as RVE countermeasures in two recent bed rest studies, BBR-1 and BBR-2 (Fig. 2.22), described in previous paragraphs for normal but also disused skeletal muscle over other standard physical exercise protocols probably is the combination between low-frequency-controlled resistive loading stimuli targeted to individual muscles or groups (to maintain muscle mass) and to induce adequate neuromuscular activation (to maintain responsiveness of motor units) thereby addressing two of the well-known structural and functional negative outcomes following extended periods of disuse on Earth or in Space (Edgerton et al. 2001).

In principle, vibration signals of the RVE protocol are transmitted by an alternating tilted foot platform to individual muscles or groups of muscles of the human body either in normal standing/squatting position or even in supine body position for only short training intervals (3–5 min) on the ground (Fig. 2.23). The mechanical and neuronal signals thus triggered are equivalent to the biodynamical processing mechanisms during normal muscle activity control, for example, in human posture and gait control (Ritzmann et al. 2014), that is spontaneously triggered almost automatically in a physiological way by preprogrammed spinal reflex control mechanisms. If combined with standard exercise protocols, this new physiological exercise modality has the capacity to improve the training outcome particularly for postural muscle groups compared which often require strenuous and powerful training bouts with maximally strength output with a strong compliance and level of motivation needed for users during longer training sessions for success. This may be of particular importance for the health and fitness and rehabilitation of older adults and other special populations but more and more also for the younger generation, thus facing sedentary lifestyles. Currently, frequency-controlled whole body vibration is considered to serve as an adequate physiological trigger to support neuromusculoskeletal structure and function and to stabilize muscle endurance critical to body gait and postural control (Rittweger 2010).

In view of alternative and more efficient physical exercise protocols as countermeasure to skeletal muscle disuse atrophy, resistive vibration exercise (RVE) was successfully tested to support muscle and bone quality and to mitigate a number of different disuse atrophy changes in two ESA long-term bed rest studies performed at the Charité Berlin, Germany (Rittweger et al. 2006; Blottner et al. 2006; Mulder et al. 2006; Belavý et al. 2009, 2012; Miokovic et al. 2011; Buehring et al. 2011). In principle RVE is able to address either individual muscle groups or functional

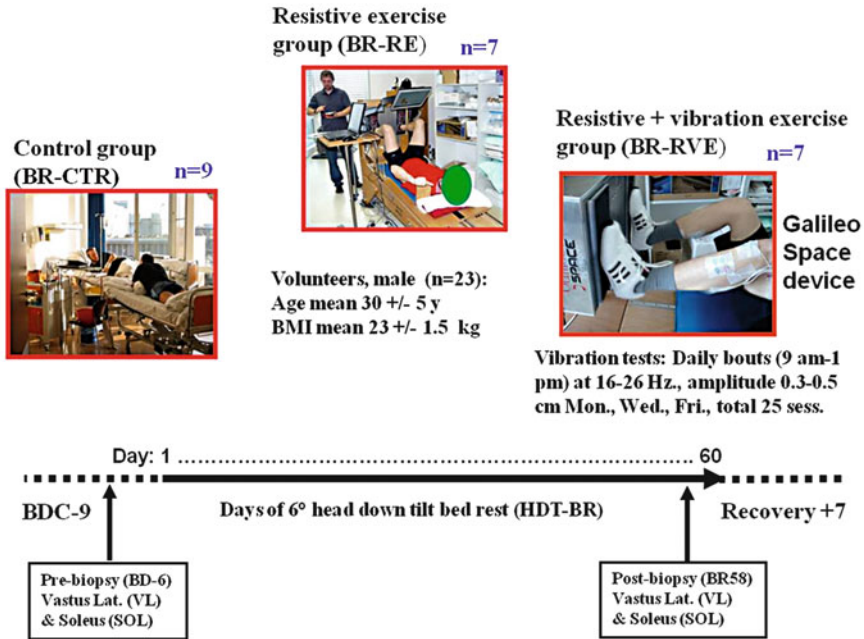


Fig. 2.23 Scenario of the 60 days BBR-2 bed rest study performed at the Charité Berlin, Germany, in 2006/2007 with three study groups, one supine control (BR-CTR) bed rest-only without exercise, one bed rest resistive exercise group (BR-RE), and one bed rest resistive exercise superimposed by vibration (BR-RVE). The muscle biopsy was taken at baseline data control (BDC-6) before bed rest and shortly before end (BR + 58) of the bed rest period. For the BBR-2 study protocols, see Belavý et al. 2010

chains of muscles (arms or legs) or to address global muscle groups of the whole human body depending on the training objectives (www.galileo-training.com). As pointed out already in the introductory paragraph, whole body vibration (RVE) is based on relatively short intervals (3–5 min) of low-frequency mechanical impulses (<20–30 Hz) with moderate amplitudes (0.5–1 cm) produced by a tilted vibrating platform for use in upright body position (Galileo®) or at supine body position (Galileo Space® trainer, Fig. 2.23), both designed and custom-made by a medico-technical company (Novotec Medical, Pforzheim, Germany). Unlike other training devices with vertical (up and down) movements, the Galileo tilted plate movements simulate human gait in a physiological way because of a side-alternating acceleration of the legs, pelvis, and lumbar spine and their individual extensor and flexor muscles (www.galileo-training.com).

The muscle contractions thus induced by frequencies starting from about 12 Hz onward are considered to be controlled by neuroreflexive mechanisms (spontaneously contractions executed via H-reflex-based afferent/efferent stimulation upon mechanical stretch signals, Kramer et al. 2013) rather than by voluntary muscle activation (voluntarily, contractions are executed by arbitrary/planned channeling

from higher brain areas to efferent spinal motor activity). Because RVE makes use of preprogrammed muscle activation at the spinal cord level (spinal reflexes), the work-out efficiency (training effects) may be less influenced by the compliance/motivation of users (e.g., users with reduced drive for motions) compared to other standard RE protocols to counteract disuse atrophy that usually require a strong mental focus on maximal power and force production during the training bouts (particularly in more or less fully body relaxation in bed rest and in spaceflight). Short RVE training intervals with, for example, 25 Hz for 3 min produce muscle stretch reflex contractions equivalent to about 4500 steps (www.galileo-training.com) which is about half of the battle with regard to the number of total steps recommended for daily physical activity in apparently healthy sedentary and older populations on Earth (Zehr and Stein 1999; Abdelmoity et al. 2000; Tudor-Locke et al. 2011).

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